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Spillman, Jr. et al.

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(54) **SYSTEM, DEVICE, AND METHOD FOR
DETECTING PERTURBATIONS VIA A FIBER
OPTIC SENSOR**

(58) **Field of Classification Search** 250/227.14,
250/227.15, 227.19; 385/13; 356/73.1
See application file for complete search history.

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(*) **Notice:** Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 61 days.

This patent is subject to a terminal dis-
claimer.

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(22) **PCT Filed:** **Nov. 17, 2003**

Primary Examiner—Thanh X. Luu

(86) **PCT No.:** **PCT/US03/36680**

(74) *Attorney, Agent, or Firm*—Michael Haynes PLC;
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(2), (4) **Date:** **May 11, 2005**

(57) **ABSTRACT**

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PCT Pub. Date: **Mar. 6, 2004**

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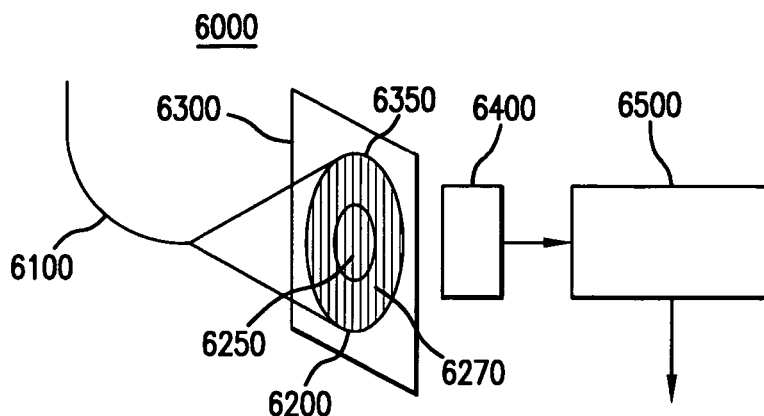
Related U.S. Application Data

(60) **Provisional application No.** 60/427,683, filed on Nov.
18, 2002.

(51) **Int. Cl.**
G01J 1/04 (2006.01)

(52) **U.S. Cl.** 250/227.14; 385/13

80 Claims, 23 Drawing Sheets



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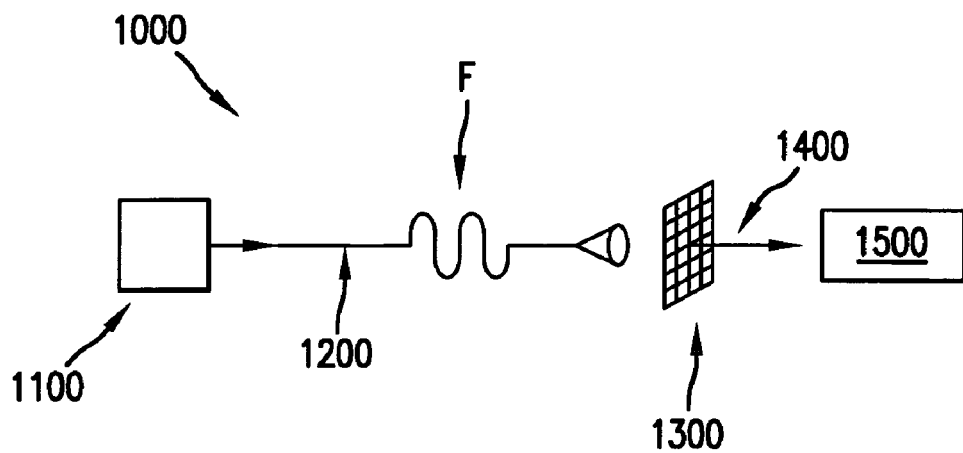


FIG. 1

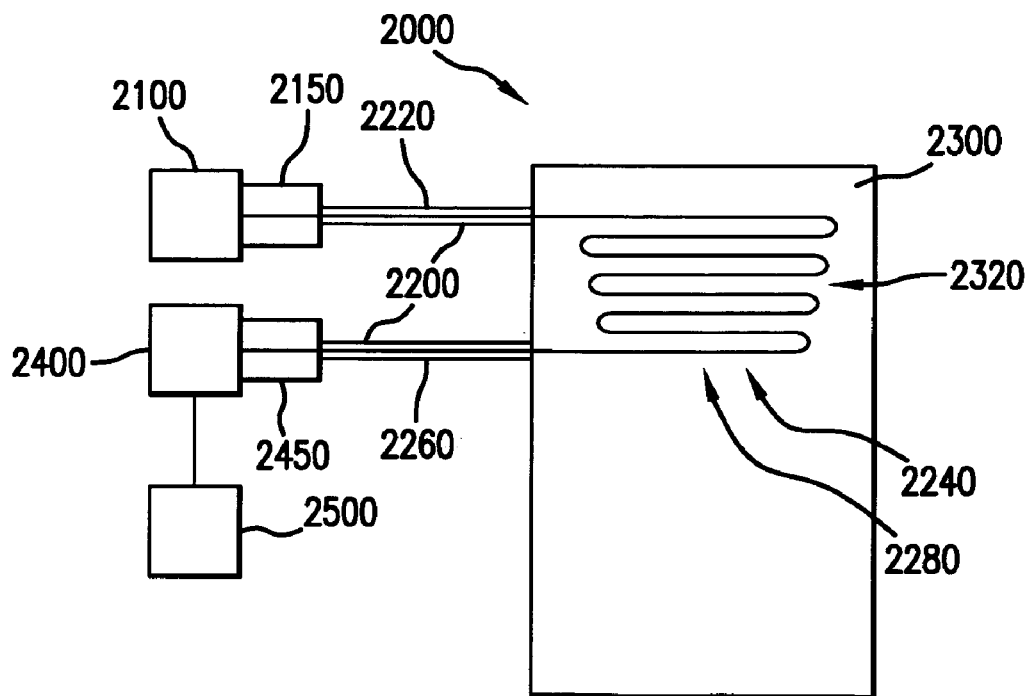


FIG. 2

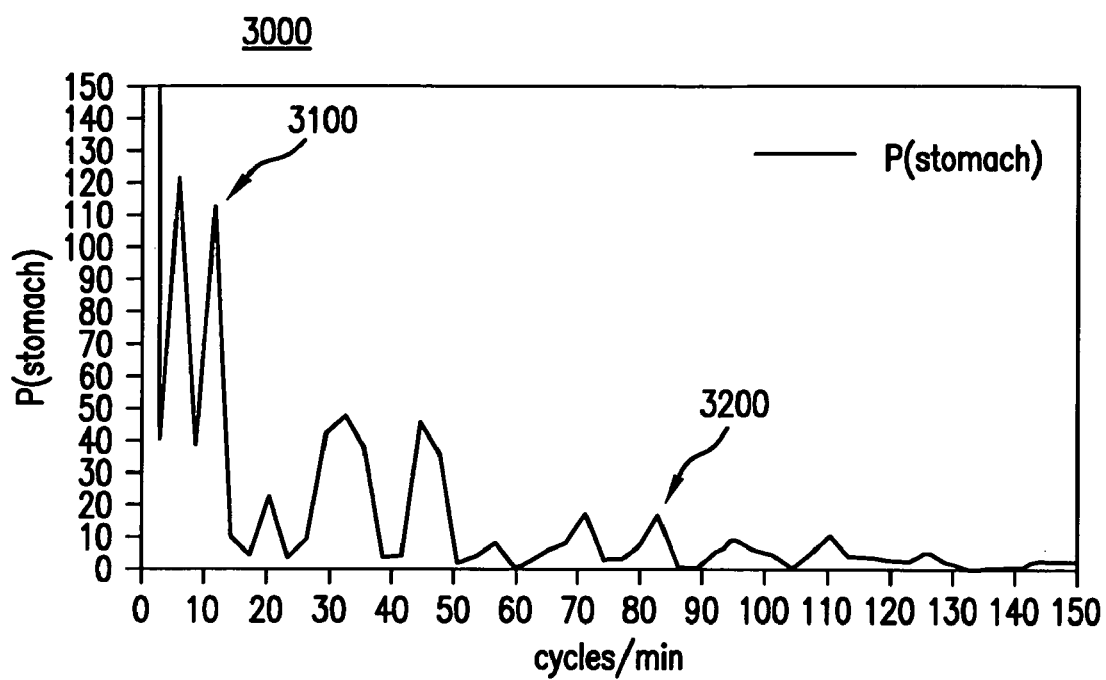


FIG.3

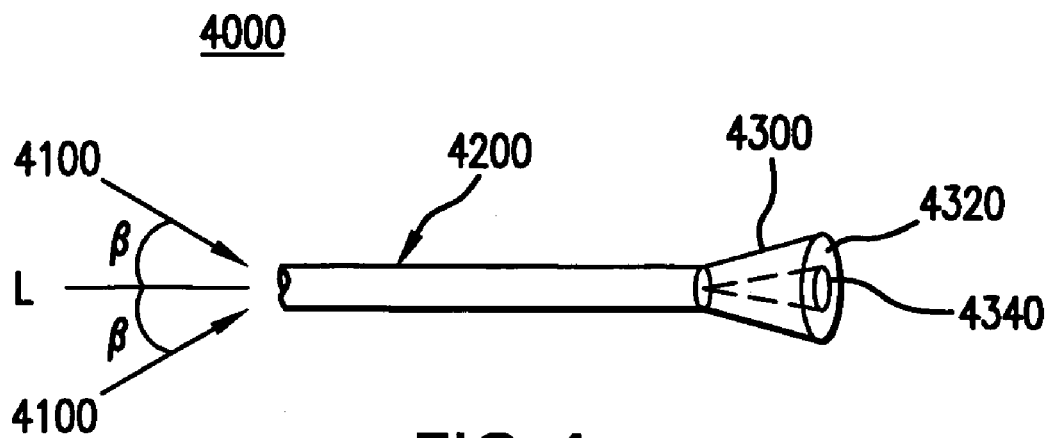


FIG. 4

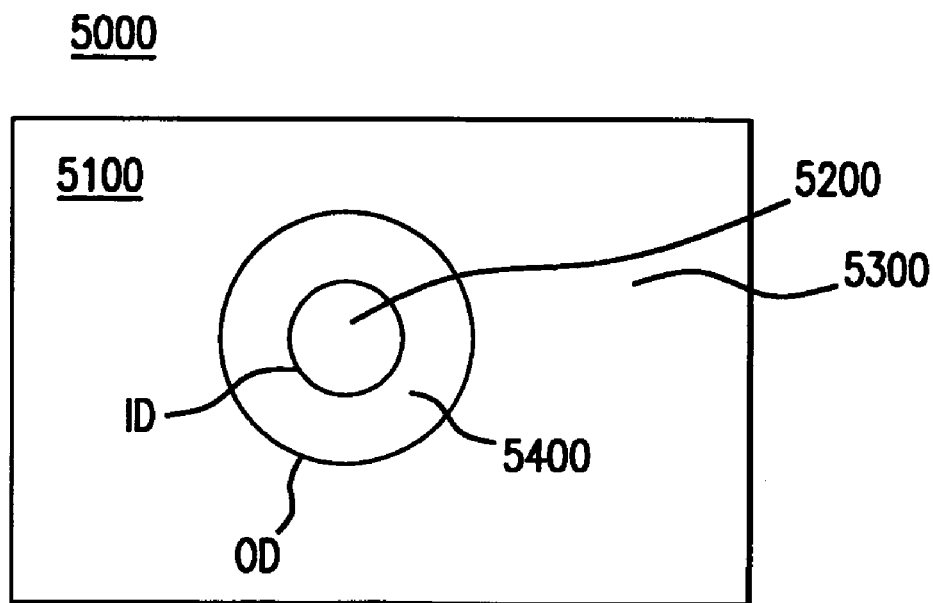


FIG. 5

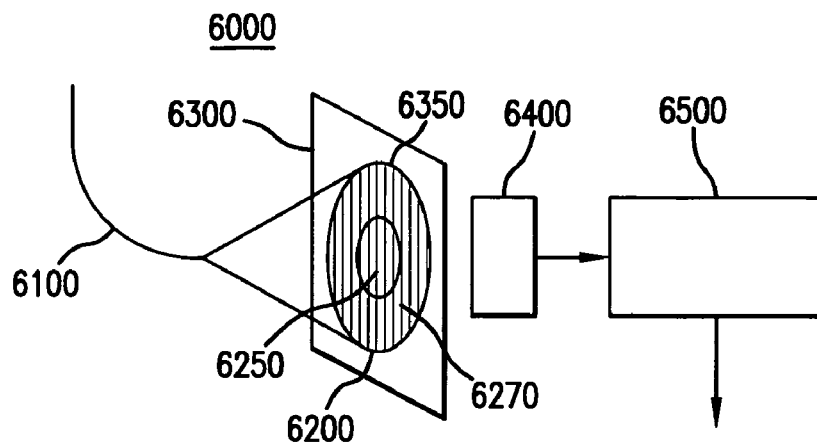


FIG. 6

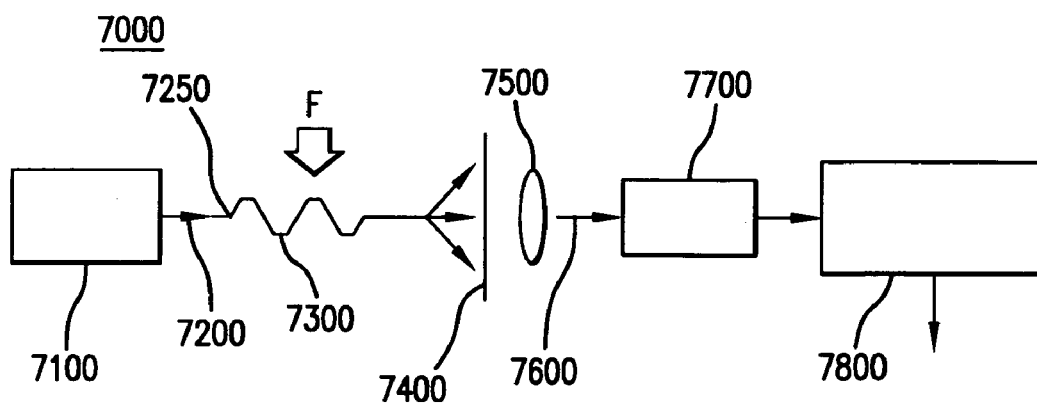


FIG. 7

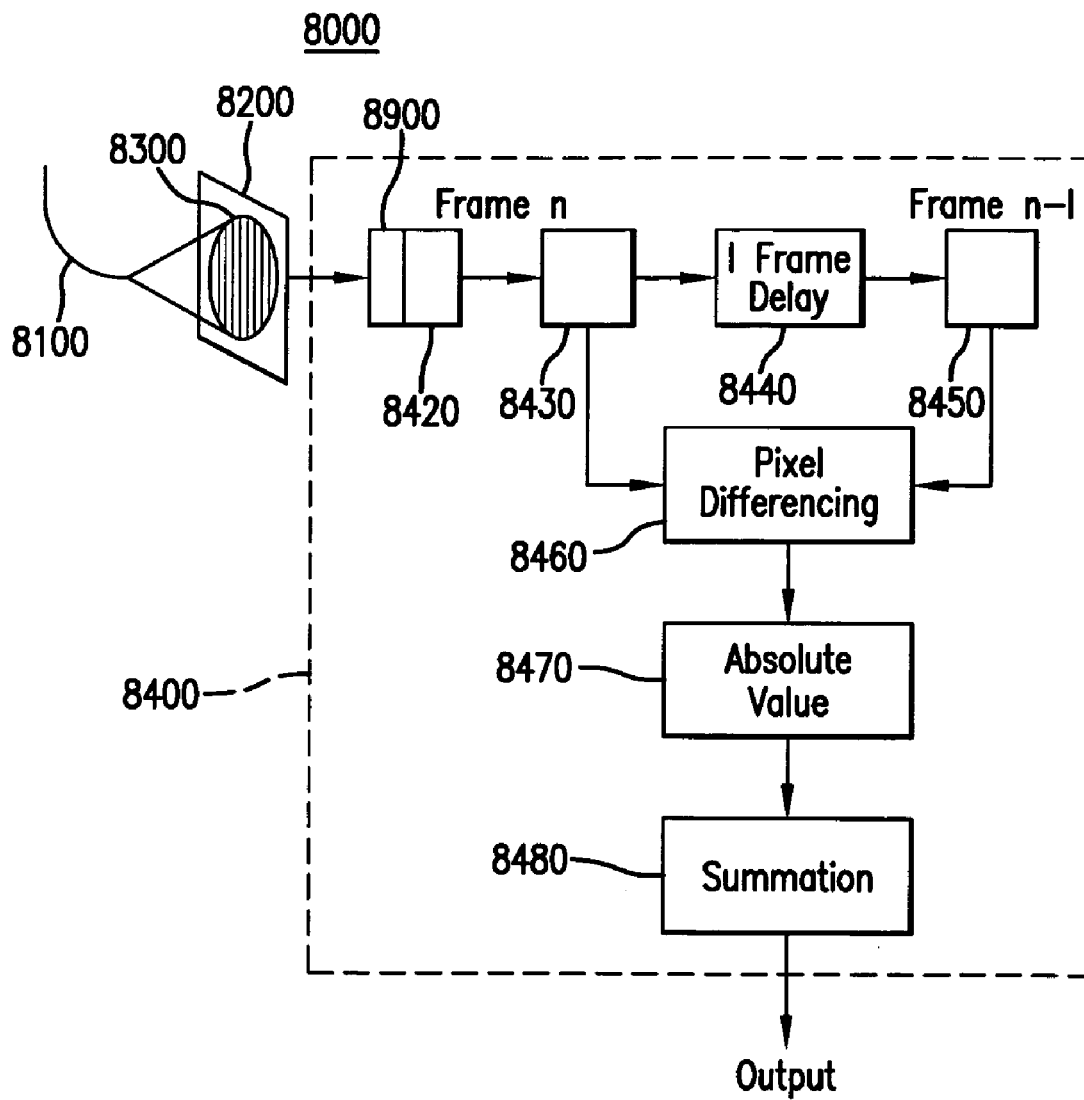


FIG.8

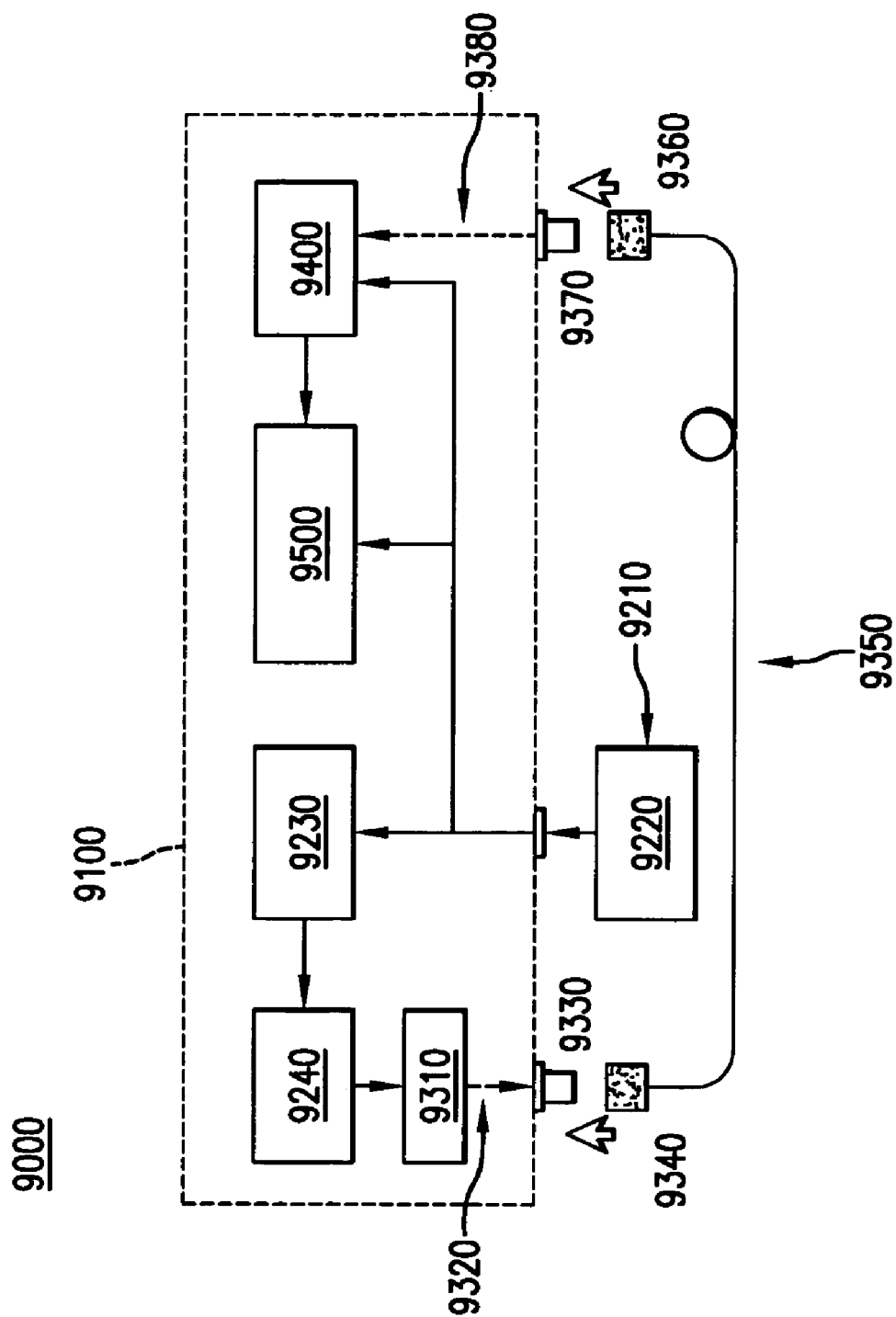


FIG. 9

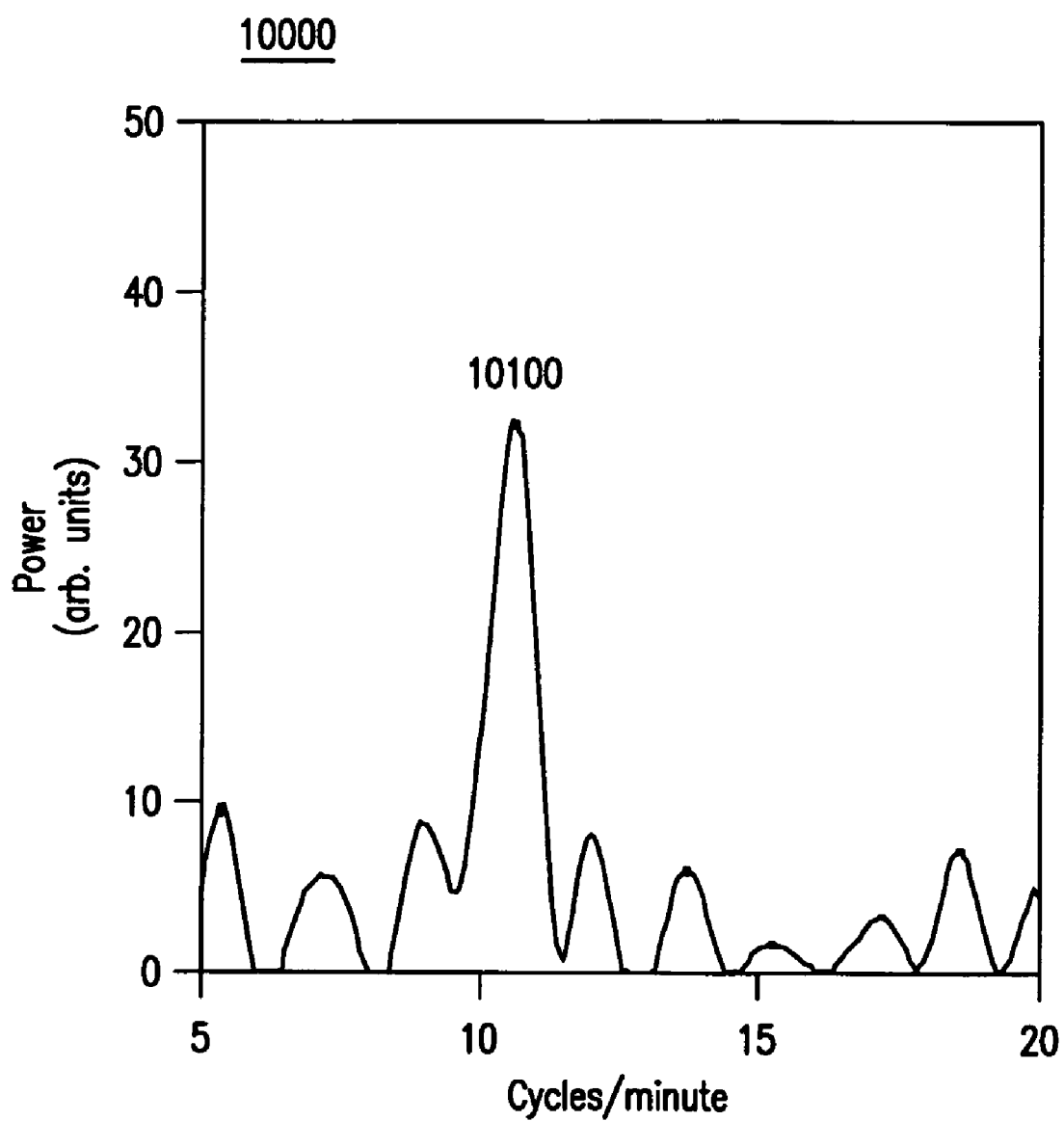


FIG. 10

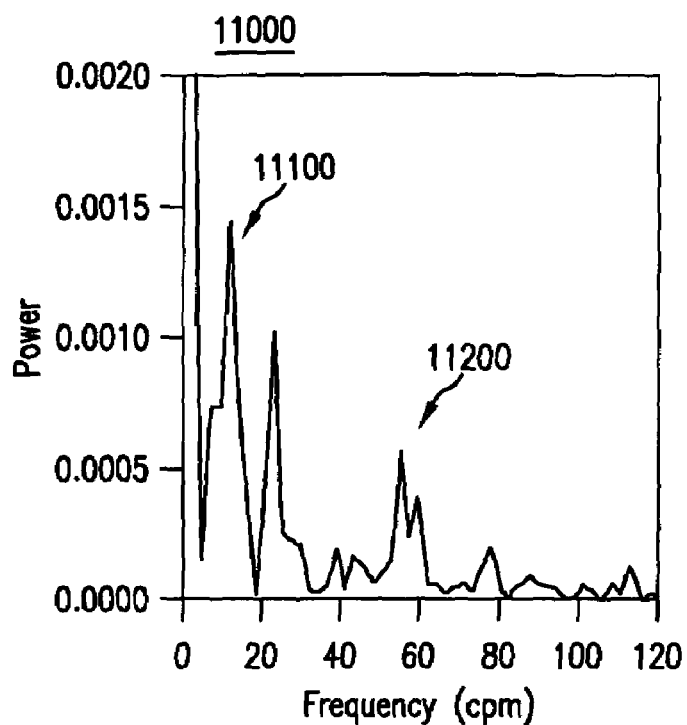


FIG. 11

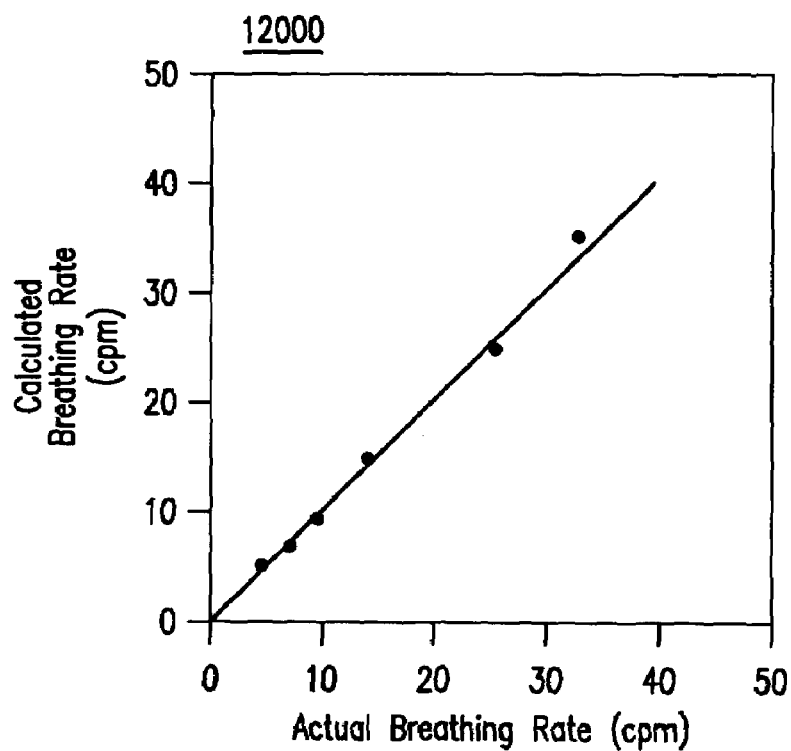


FIG. 12

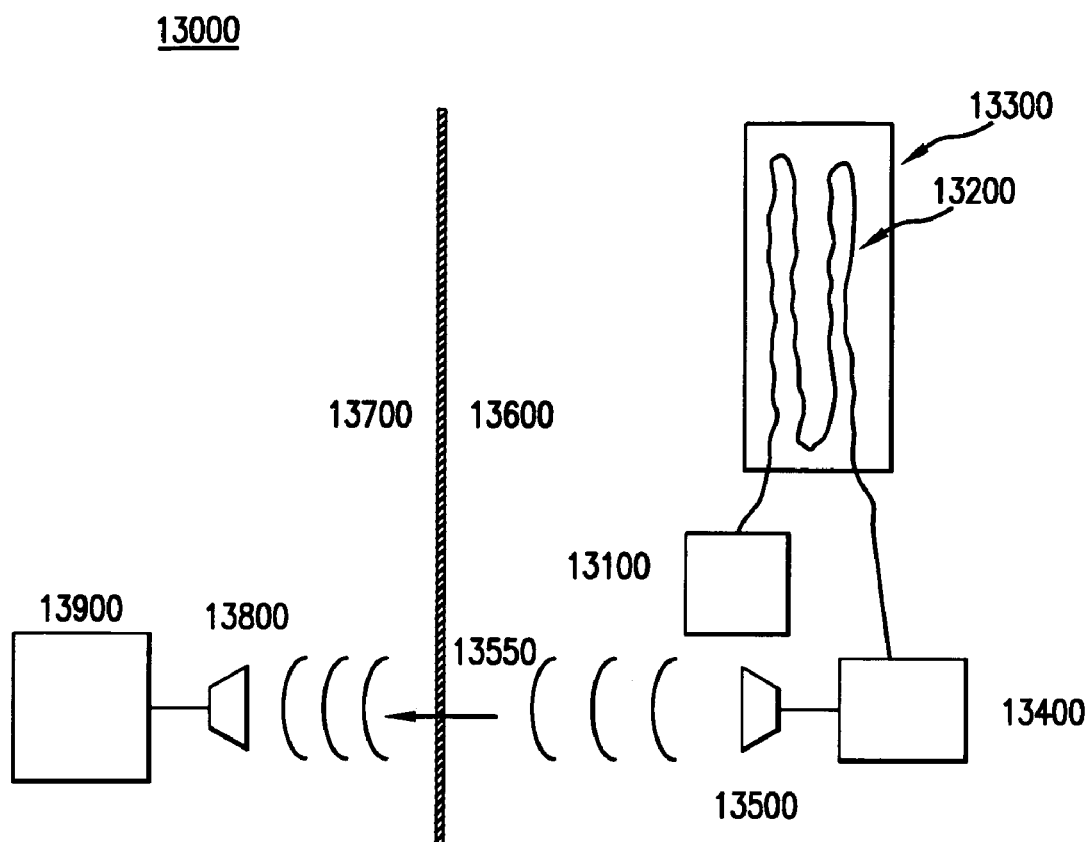


FIG.13

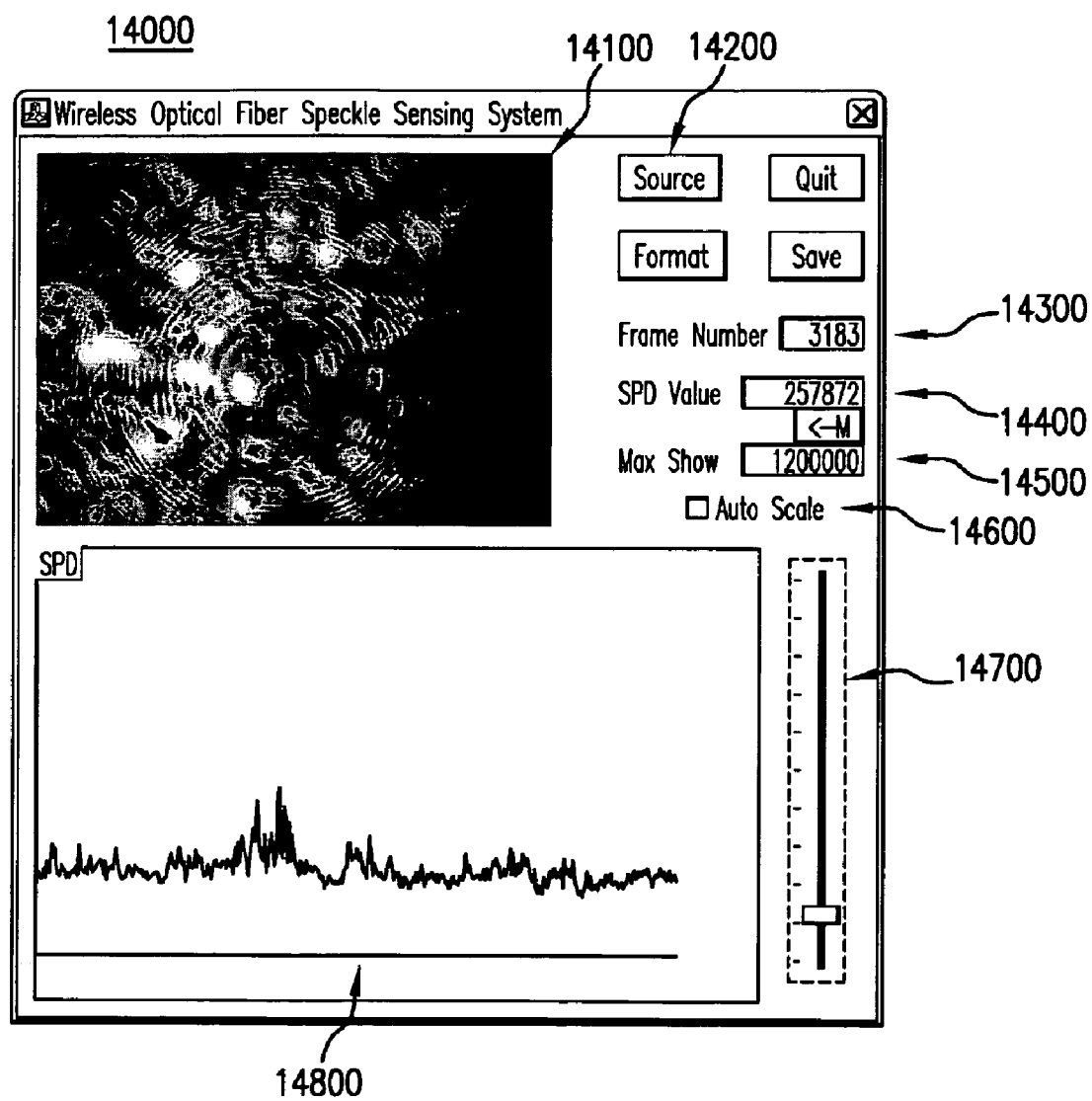


FIG. 14

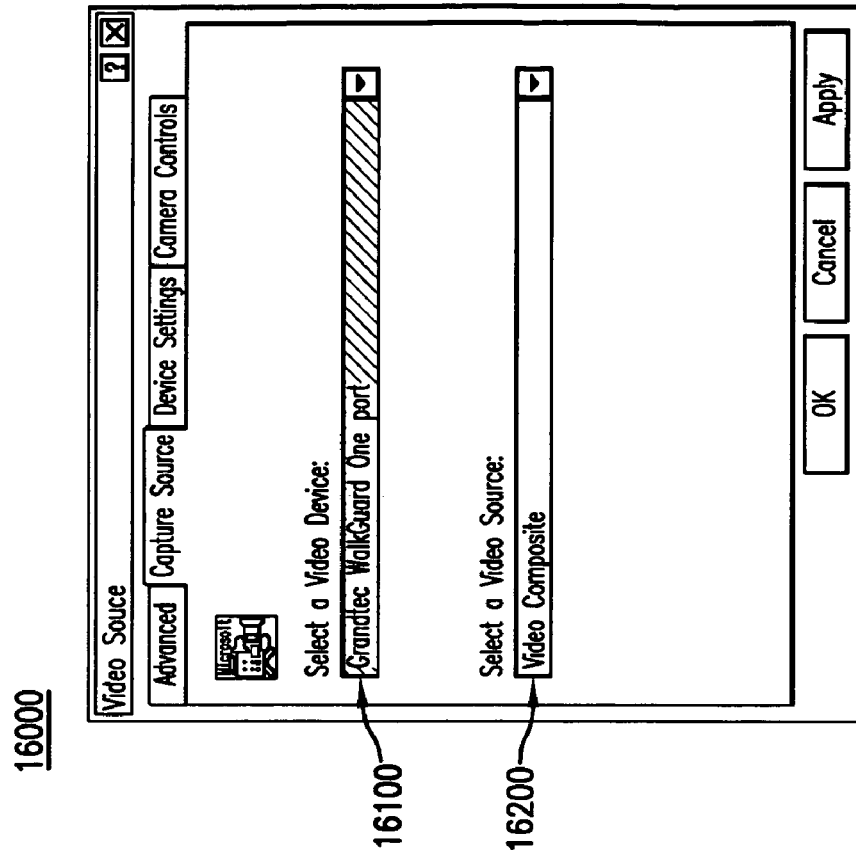


FIG. 16

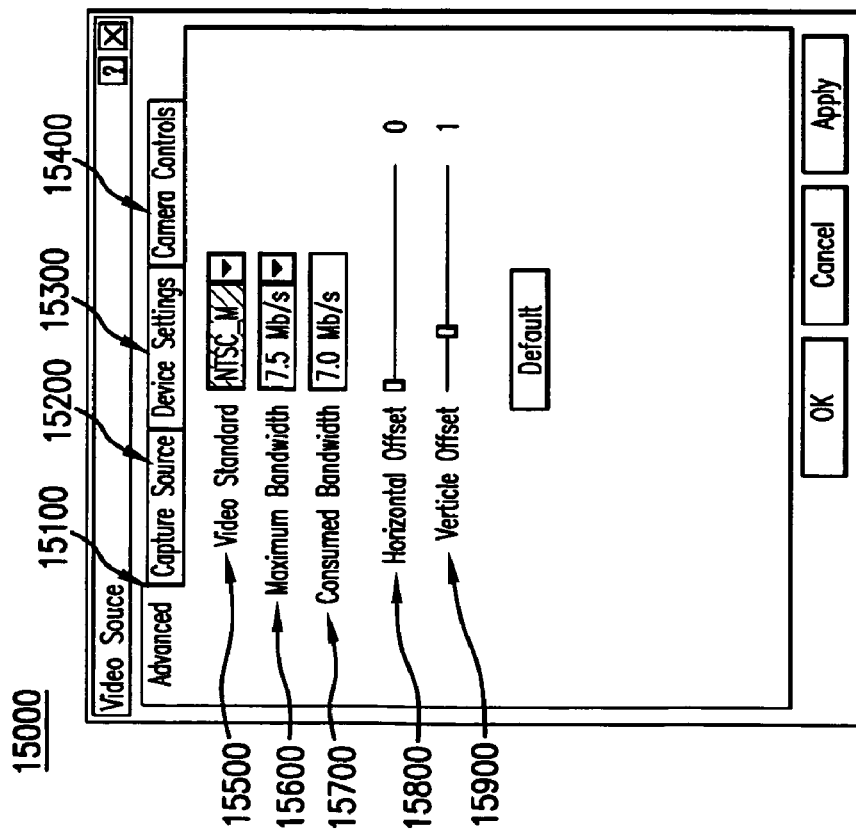


FIG. 15

17000

FIG. 17 is a screenshot of a 'Video Source' settings window. The window has a title bar with a question mark icon and a close button. Below the title bar are four tabs: 'Advanced', 'Capture Source', 'Device Settings', and 'Camera Controls'. The 'Device Settings' tab is currently selected. It contains a list of image quality controls, each with a slider and a 'Value' field. The controls are: Brightness (Value: 16), Contrast (Value: 16), Hue (Value: 16), Saturation (Value: 16), Sharpness (Value: 0), White balance (Value: 0), Gamma (Value: 0), and Backlight Comp (Value: 0). A 'Default' button is located below the sliders. At the bottom right are 'OK', 'Cancel', and 'Apply' buttons.

Control	Value	Auto
Brightness	16	<input type="checkbox"/>
Contrast	16	<input type="checkbox"/>
Hue	16	<input type="checkbox"/>
Saturation	16	<input type="checkbox"/>
Sharpness	0	<input type="checkbox"/>
White balance	0	<input type="checkbox"/>
Gamma	0	<input type="checkbox"/>
Backlight Comp	0	<input type="checkbox"/>

FIG. 17

18000

FIG. 18 is a screenshot of a 'Video Source' settings window, similar to FIG. 17 but with the 'Camera Controls' tab selected. The controls are: Zoom (Value: 100), Focus (Value: 0), Exposure (Value: 0), Iris (Value: 0), Tilt (Value: 0), Pan (Value: 0), and Roll (Value: 0). Each control has a slider and a 'Value' field. At the bottom right are 'OK', 'Cancel', and 'Apply' buttons.

Control	Value	Auto
Zoom	100	<input type="checkbox"/>
Focus	0	<input type="checkbox"/>
Exposure	0	<input type="checkbox"/>
Iris	0	<input type="checkbox"/>
Tilt	0	<input type="checkbox"/>
Pan	0	<input type="checkbox"/>
Roll	0	<input type="checkbox"/>

FIG. 18

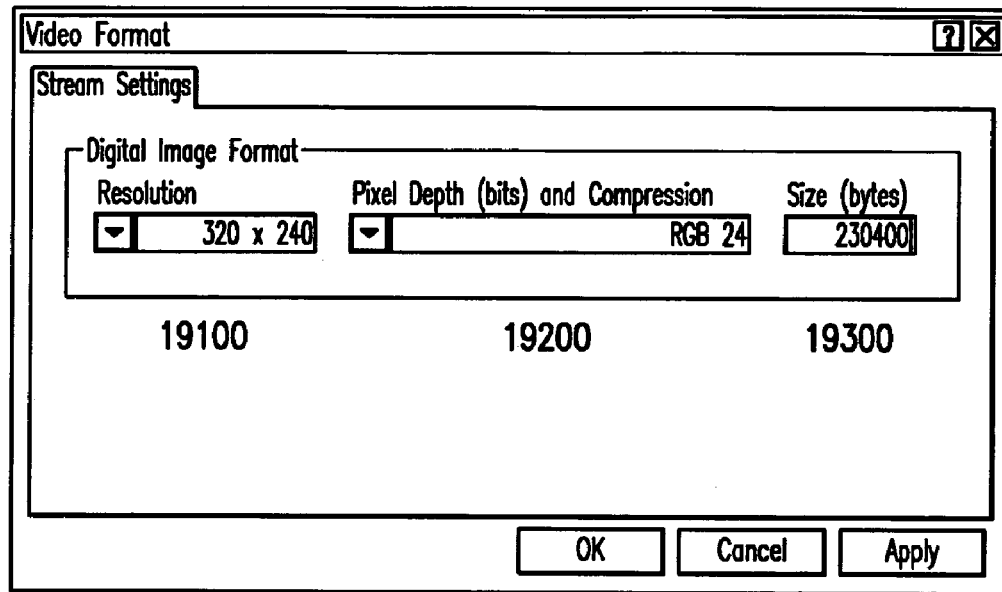
19000

FIG.19

20000

20100

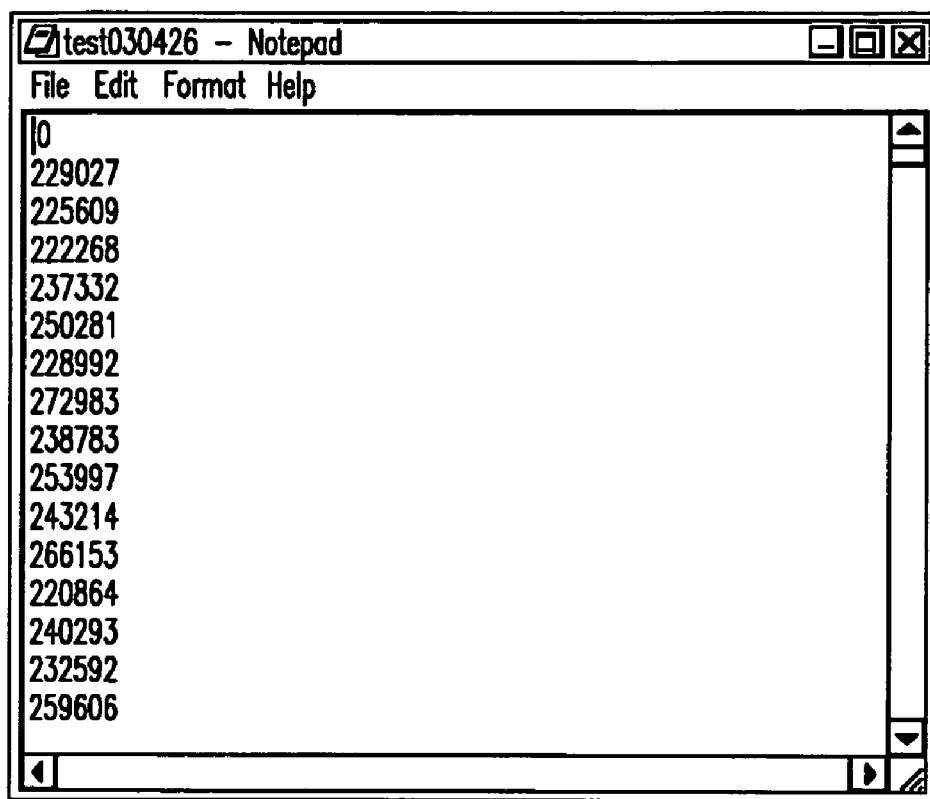


FIG.20

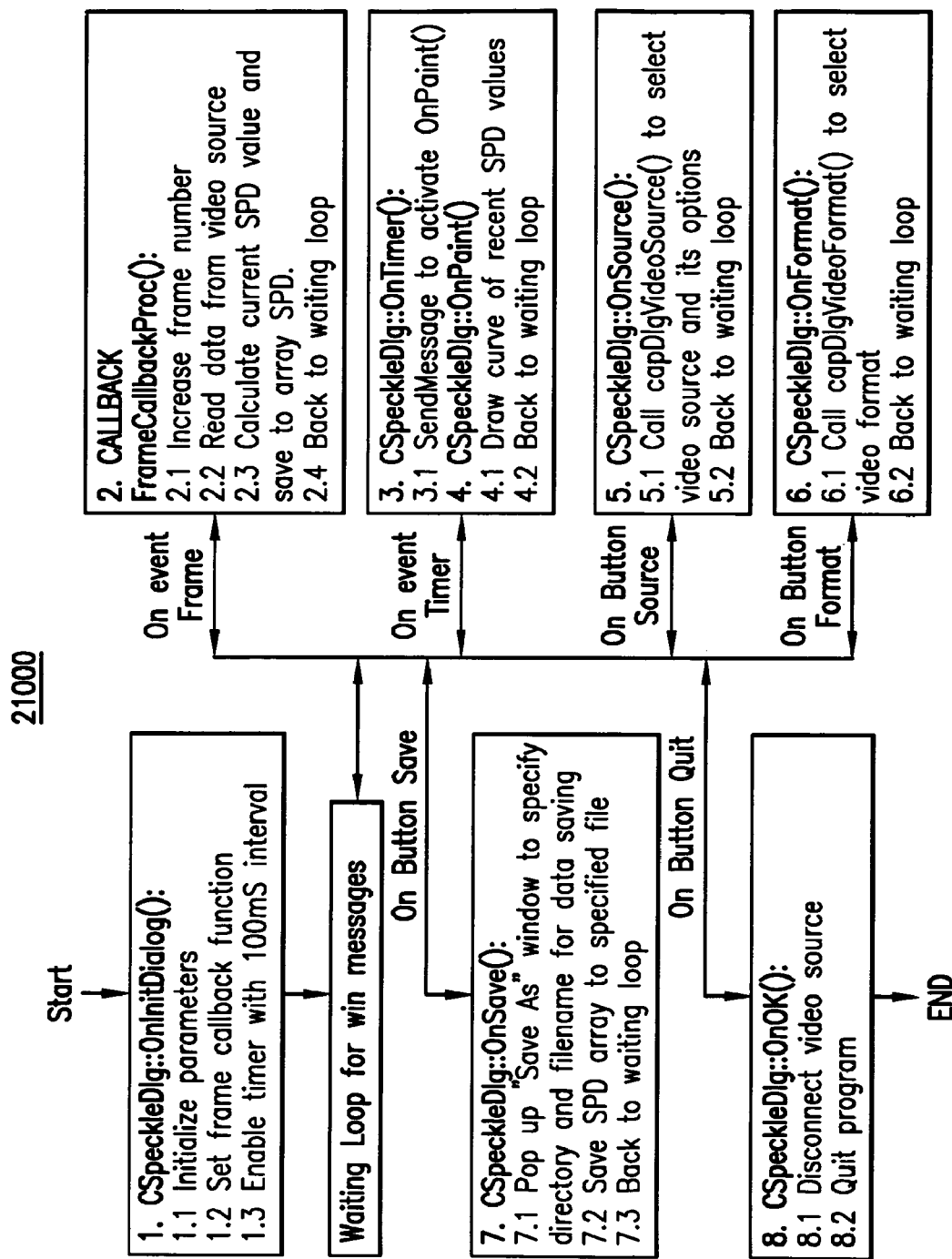


FIG. 21

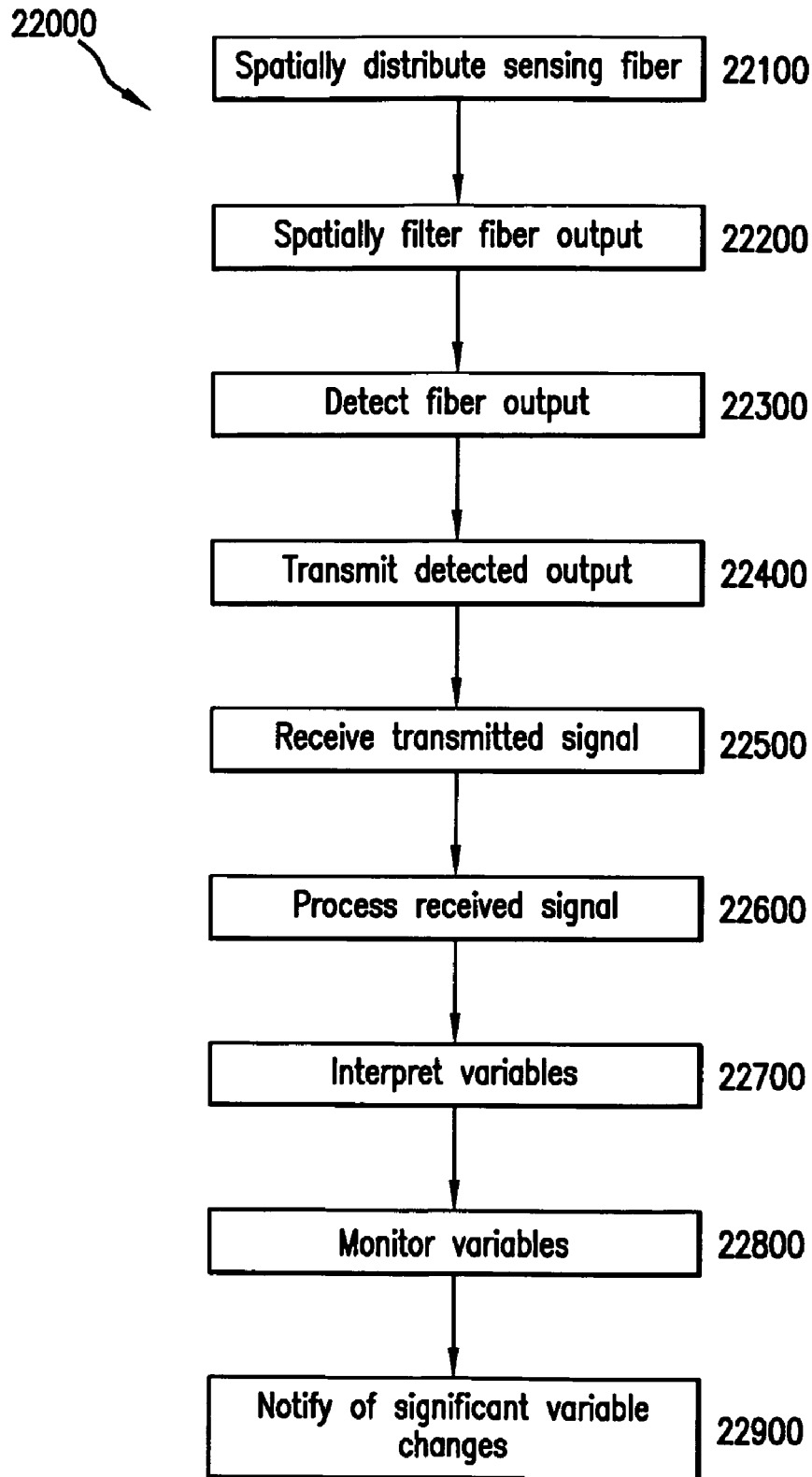


FIG.22

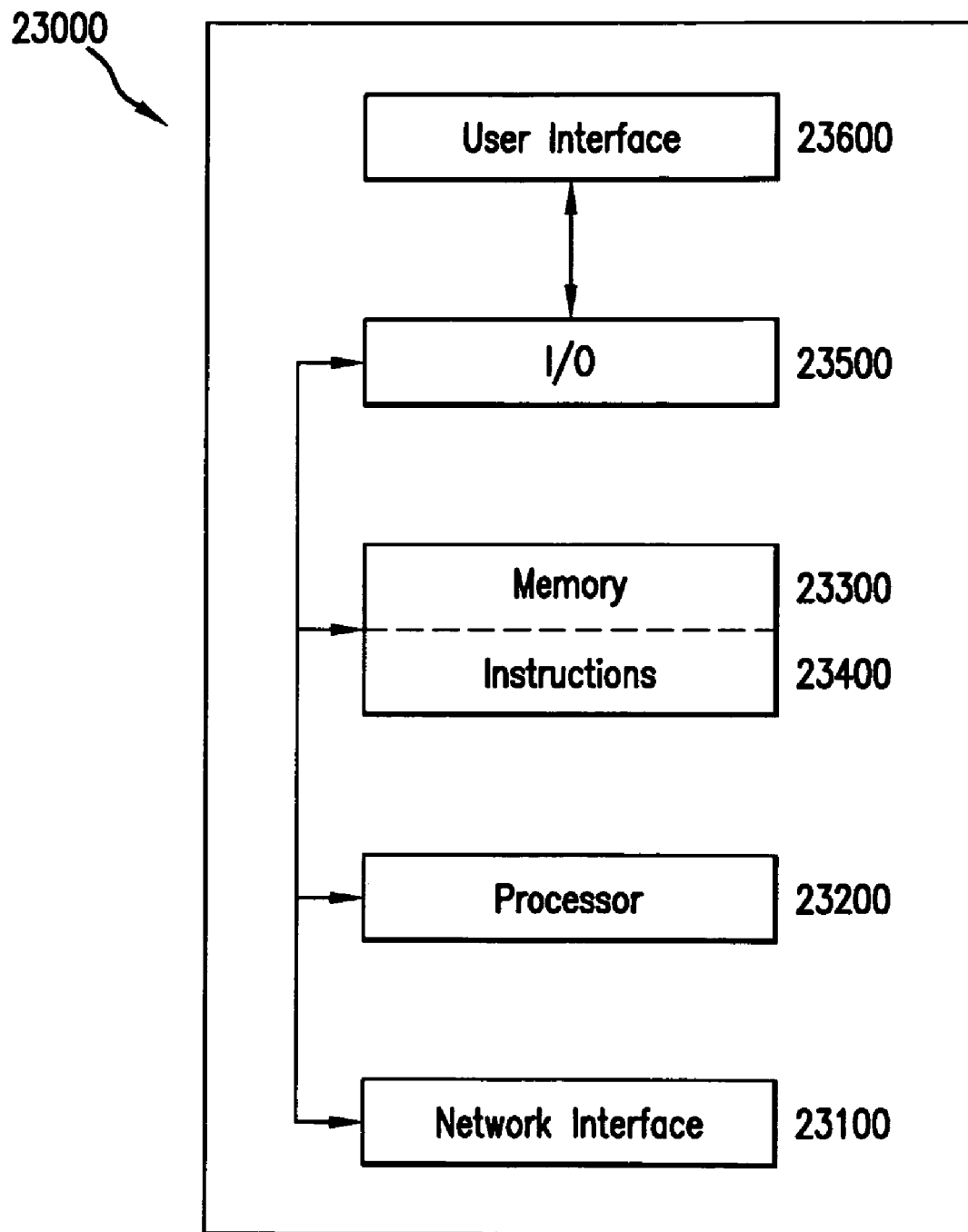


FIG. 23

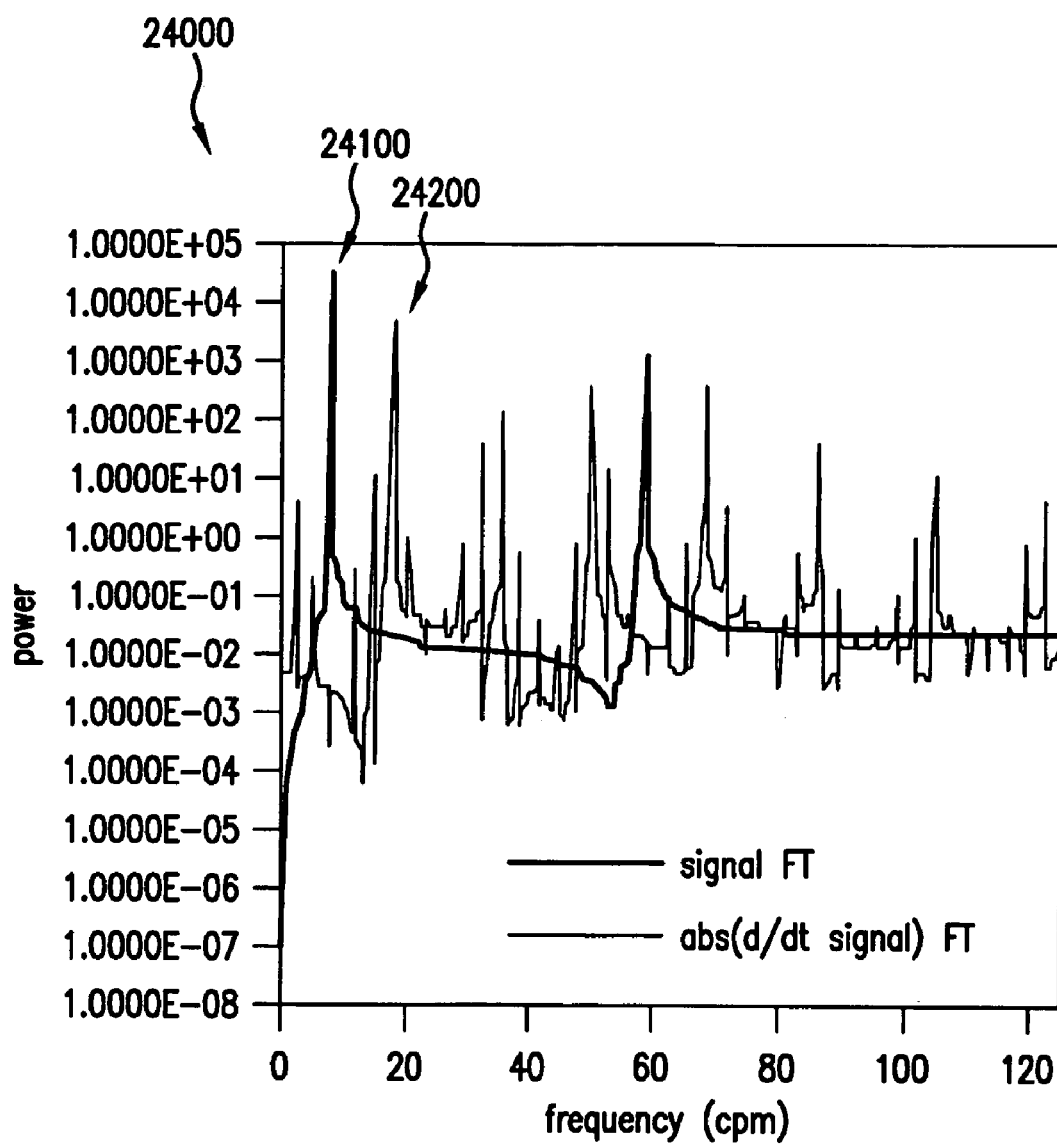


FIG.24

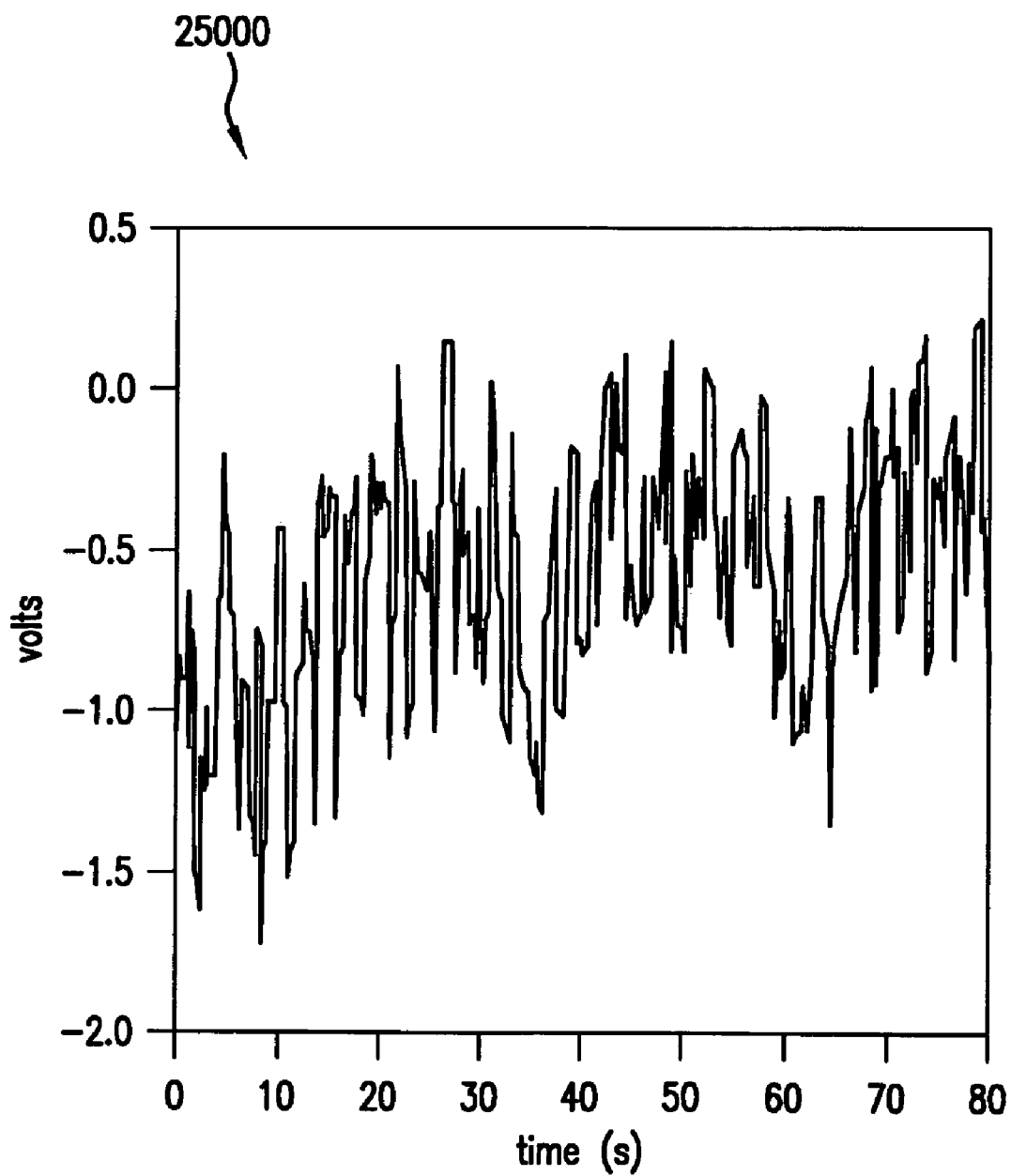


FIG.25

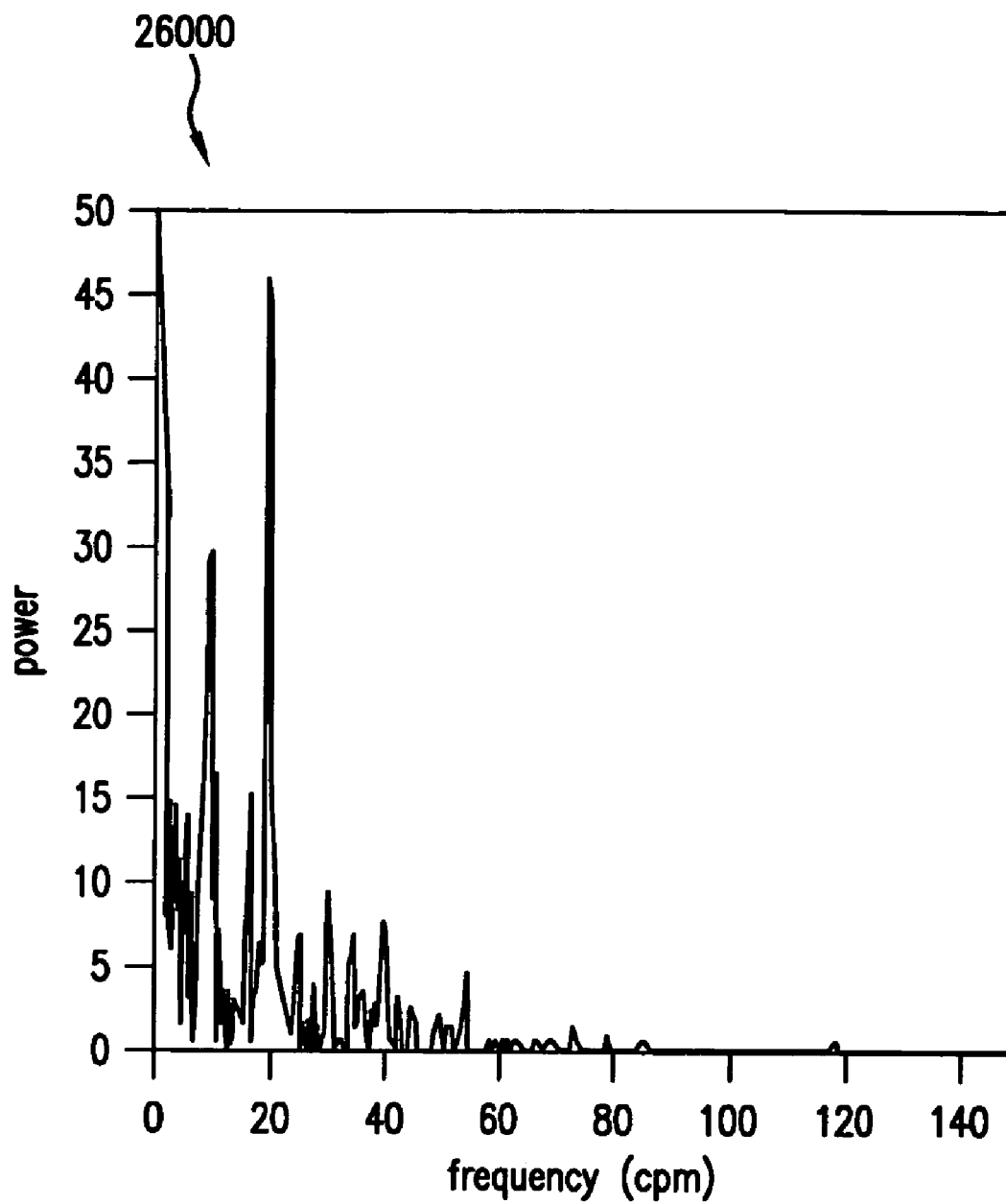


FIG.26

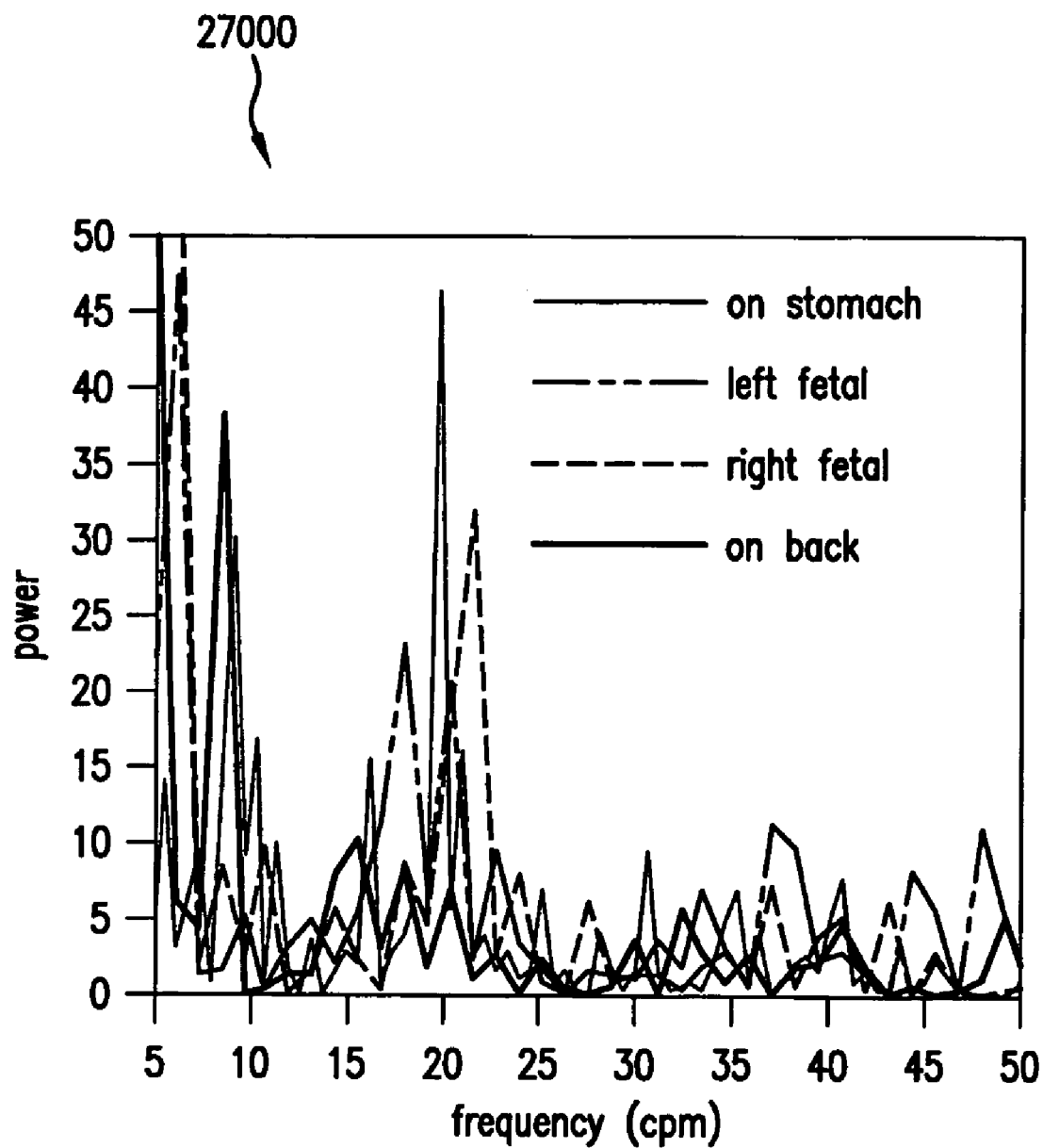


FIG.27

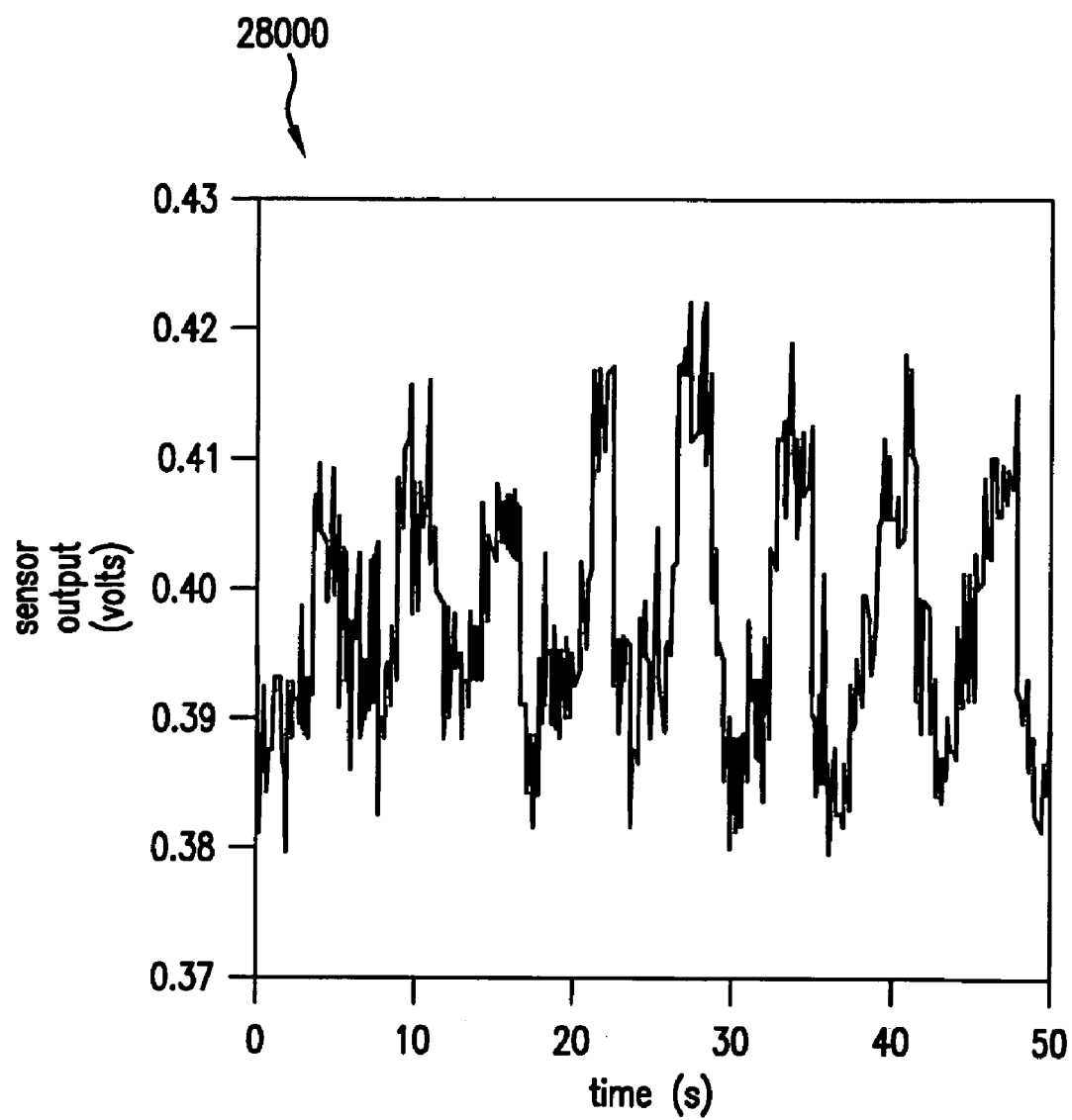


FIG. 28

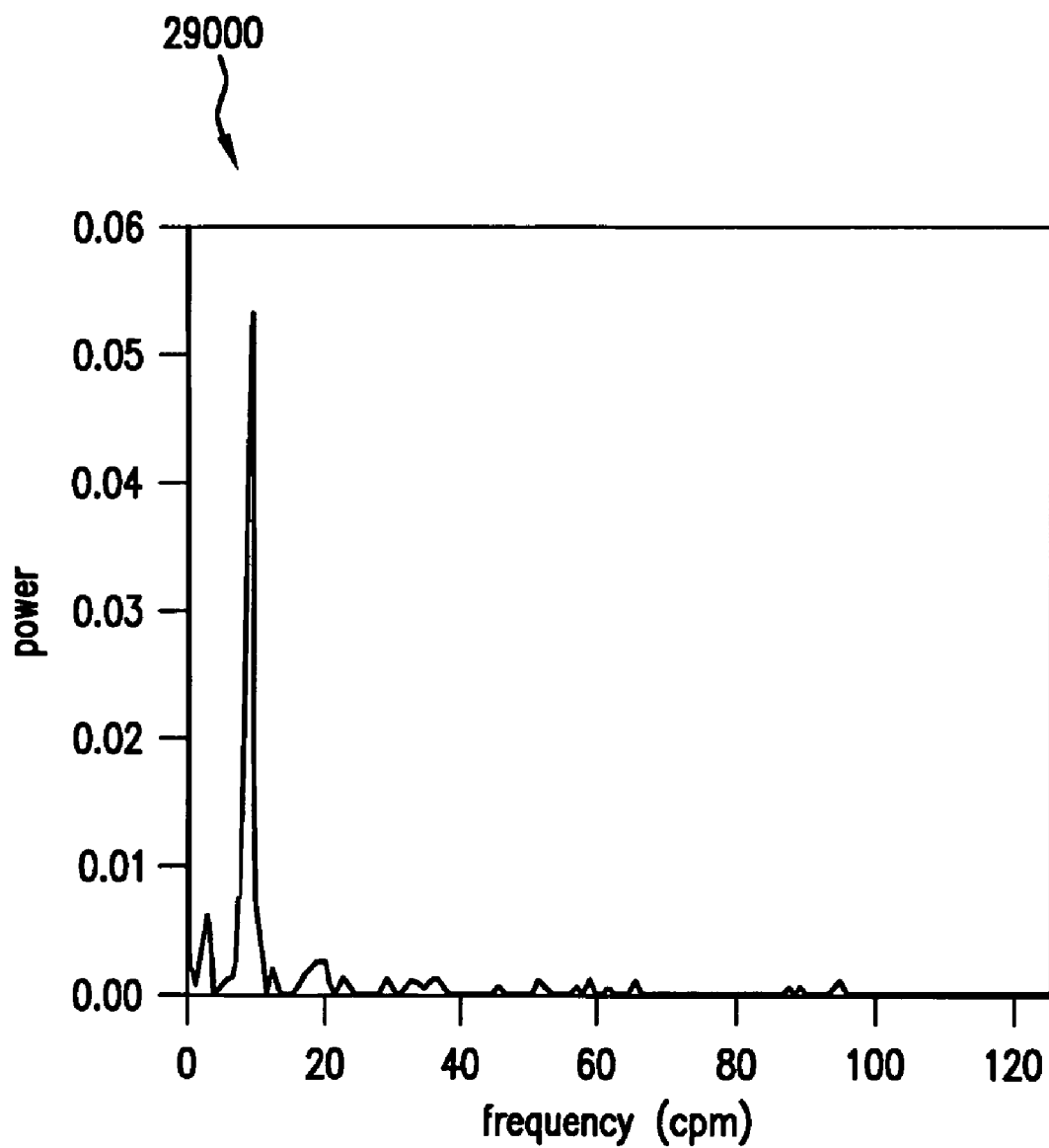


FIG.29

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SYSTEM, DEVICE, AND METHOD FOR DETECTING PERTURBATIONS VIA A FIBER OPTIC SENSOR

CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims priority to, and incorporates by reference in its entirety, pending U.S. Provisional Patent Application Ser. No. 60/427,683, filed 18 Nov. 2002.

BRIEF DESCRIPTION OF THE DRAWINGS

A wide array of potential embodiments can be better understood through the following detailed description and the accompanying drawings in which:

FIG. 1 is a block diagram of an exemplary embodiment of a multimode fiber optic sensor;

FIG. 2 is a block diagram of an exemplary embodiment of an integrated monitoring device;

FIG. 3 is a Fourier transform of data generated by a test subject lying on her stomach in an exemplary embodiment of an integrated monitoring bed depicted in FIG. 2;

FIG. 4 is a side view of an exemplary embodiment of a multimode optic fiber;

FIG. 5 is a front view of a projection on a flat screen of an output from the exemplary embodiment of FIG. 4;

FIG. 6 is a block diagram of an exemplary embodiment of a system **6000**;

FIG. 7 is a block diagram of an exemplary embodiment of a system **7000**;

FIG. 8 is a block diagram of an exemplary embodiment of a system **8000**;

FIG. 9 is a block diagram of an exemplary embodiment of a system **9000**;

FIG. 10 is a plot of power versus frequency data generated by an exemplary embodiment of the optical fiber sensor of FIG. 6;

FIG. 11 is a plot of power versus frequency data generated by an exemplary embodiment of the optical fiber sensor of FIG. 6;

FIG. 12 is a plot correlating calculated respiration rate vs. actual breathing rate for data gathered via an exemplary embodiment of the optical fiber sensor of FIG. 6;

FIG. 13 is a block diagram of an exemplary embodiment of a system **13000**;

FIG. 14 is an exemplary user interface **14000** for a wireless optical fiber speckle sensing system;

FIG. 15 is an exemplary user interface **15000**;

FIG. 16 is an exemplary user interface **16000**;

FIG. 17 is an exemplary user interface **17000**;

FIG. 18 is an exemplary user interface **18000**;

FIG. 19 is an exemplary user interface **19000**;

FIG. 20 is an exemplary output data list **20000**;

FIG. 21 is structural diagram of an exemplary software program **21000**;

FIG. 22 is a flowchart of an exemplary embodiment of a method **22000**;

FIG. 23 is a block diagram of an exemplary embodiment of an information device **23000**;

FIG. 24 is a plot of a power spectra of two exemplary perturbation detections;

FIG. 25 is a plot of an exemplary time trace from an exemplary embodiment of an SMS sensor;

FIG. 26 is a plot of a power spectra of the signal of FIG. 25;

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FIG. 27 is a plot of an exemplary power spectra for different positions;

FIG. 28 is a plot of an exemplary time trace from an exemplary embodiment of a HOME sensor; and

FIG. 29 is a plot of a power spectra of the signal of FIG. 28.

DEFINITIONS

When the following terms are used herein, the accompanying definitions apply.

optical fiber—a filament of transparent dielectric material, usually glass or plastic, and usually circular in cross section, that guides light. An optical fiber usually has a cylindrical core surrounded by, and in intimate contact with, a cladding of similar geometry. So that the light can be guided by the fiber, the refractive index of the core is slightly different than that of the cladding.

fiber optic sensor—a device that utilizes an optical fiber as a transducer.

transducer—a device that converts one form of energy into another. For example, a sensing optical fiber can convert changes in mechanical energy, such as a perturbation of the fiber, to changes in optical energy.

mode—in a waveguide or cavity, one of the various possible patterns of propagating or standing electromagnetic fields. Each mode is typically characterized by angle, frequency, polarization, electric field strength, and/or magnetic field strength. For example, when a pulse of light is transmitted through an optical fiber, the energy can follow a number of paths that cross the fiber's longitudinal axis at different angles. A group of paths that cross the axis at the same angle is known as a mode.

lowest order mode—also known as the fundamental mode and the LP_{01} mode, is the mode in which light passes through an optical fiber substantially parallel to the fiber's longitudinal axis.

high order mode—any mode other than the lowest order mode.

higher order mode—a mode having a higher angle of incidence with respect to the longitudinal axis of a fiber than a another, lower order, mode.

multimode—supporting the propagation of more than one mode. A multimode optical fiber may be either a graded-index (GI) fiber or a step-index (SI) fiber.

coherent—having waves with similar direction, amplitude, and phase that are capable of exhibiting interference.

integrated—formed or united into a whole or into another entity.

integrating—providing the sum or total of; additive.

spatially distributed—arranged in a pre-determined pattern in a volume.

perturbation—a change in a physical system.

photodetector—a transducer capable of accepting an optical signal and producing an electrical signal containing the same information as in the optical signal. As used herein a photodetector can comprise a photodiode, avalanche photodiode, PIN photodiode, photocell, photoelectric cell, photoconductor, CCD, and/or a CMOS device, etc.

photodetector array—a collection of photodetectors, typically arranged in a gridlike pattern.

charge-coupled device (CCD)—a light-sensitive integrated circuit that stores and displays the data for an image in such a way that each pixel (picture element) in the image is converted into an electrical charge the intensity of which is related to a color in the color spectrum (which can be a black-and-white continuum). For a system supporting, for

example 65,535 colors, there will be a separate value for each color that can be stored and recovered. One of the two main types of image sensors used in digital cameras. When a picture is taken, the CCD is struck by light coming through the camera's lens. Each of the thousands or millions of tiny pixels that make up the CCD convert this light into electrons. The number of electrons, usually described as the pixel's accumulated charge, is measured, then converted to a digital value. This last step can occur outside the CCD, in a component called an analog-to-digital converter.

complementary metal-oxide semiconductor (CMOS)—one of the two main types of image sensors used in digital cameras. Its basic function is the same as that of a CCD.

field emitter—a device that is fabricated on a sub-micron scale with lithography technique, and that emits electrons immediately when a voltage is applied.

digital camera—a camera that captures an image not on film, but in an electronic imaging sensor that takes the place of film.

image—an at least two-dimensional representation of an object and/or phenomenon.

coupled—connected or linked by any known means, including mechanical, fluidic, acoustic, electrical, magnetic, optical, etc.

light pattern—a visible pattern, such as an interference pattern or speckle, created by combined modes of light.

spatial—relating to an area or volume.

spatial filter—a device or method for ignoring, exposing, or detecting a spatial portion of an image and/or signal.

matched spatial filtering—filtering a spatial pattern to emphasize a variable of interest.

wireless—any data communication technique that utilizes electromagnetic waves emitted by an antenna to communicate data (i.e., via an unguided medium), including such data communication techniques as sonar, radio, cellular, cellular radio, digital cellular radio, ELF, LF, MF, HF, VHF, UHF, SEF, EHF, radar, microwave, satellite microwave, laser, infrared, etc., and specifically excluding human voice radio transmissions, the data communication technique having a carrier frequency ranging from about 1 Hz to about 2×10^{14} Hz (about 200 teraHertz), including all values therebetween, such as for example, about 40 Hz, 6.010 kHz, 8.7 MHz, 800 MHz, 2.4 GHz, 4.518 GHz, 30 GHz, etc. and including all subranges therebetween, such as for example, from about 100 kHz to about 100 MHz, about 30 MHz to about 1 GHz, about 3 kHz to about 300 GHz, etc. Wireless communications can include analog and/or digital data, signals, and/or transmissions.

signal—detectable transmitted energy that can be used to carry information. Operationally, a type of message, the text of which consists of one or more letters, words, characters, symbols, signal flags, visual displays, or special sounds, with prearranged meaning and which is conveyed or transmitted by visual, acoustical, or electrical means. The information in a signal can be, for example digitally encrypted via for example, public key, PGP, and/or triple-DES, etc. As another example, the signal can be broadcast via, for example, a spread-spectrum technology such as, for example a frequency hopping or a direct-sequence spread-spectrum system.

signal processing module (signal processor)—a device for processing a signal. Signal processing activities can include formatting, source encoding, encrypting, channel encoding, multiplexing, modulating, frequency spreading, transmitting, receiving, frequency despread, demodulating, sampling, detecting, demultiplexing, channel decoding, decrypting, source decoding, synchronization, analyzing,

comparing, converting, transforming, Fourier transforming, interpreting, monitoring, and/or notifying, etc.

encode—to convert data by the use of a code, frequently one consisting of binary numbers, in such a manner that reconversion to the original form is possible. Alternatively, to append redundant check symbols to a message for the purpose of generating an error detection and/or correction code.

decode—to convert data by reversing the effect of previous encoding, and/or to interpret a code.

interpret—to make sense of and/or assign a meaning to.

vital sign—a physiological sign of life and usually an indicator of a person's general physical condition. Vital signs can include movement, blood temperature, blood pressure, body temperature, pulse rate, and/or respiratory rate, etc.

Publications

The following U.S. patents are hereby incorporated by reference herein in their entirety:

20030095263 (Varshneya) "Fiber optic interferometric vital sign monitor for use in magnetic resonance imaging, confined care facilities and in-hospital";

U.S. Pat. No. 6,498,652 (Varshneya) "Fiber optic monitor using interferometry for detecting vital signs of a patient";

U.S. Pat. No. 5,291,013 (Nafarrate) "Fiber optical monitor for detecting normal breathing and heartbeat motion based on changes in speckle patterns";

U.S. Pat. No. 5,212,379 (Nafarrate) "Fiber optical monitor for detecting motion based on changes in speckle patterns";

U.S. Pat. No. 5,134,281 (Bryenton) "Microbend optic sensor with fiber being sewn thereto in a sinuously looped disposition";

U.S. Pat. No. 5,436,444 (Rawson) "Multimode optical fiber motion monitor with audible output";

U.S. Pat. No. 4,863,270 (Spillman) "Multi-mode optical fiber sensor and method";

U.S. Pat. No. 4,843,233 (Jeunhomme) "Device for detecting vibrations including a multimode optical fiber as sensitive element"; and

U.S. Pat. No. 4,297,684 (Butter) "Fiber optic intruder alarm system".

DETAILED DESCRIPTION

Certain exemplary embodiments provide a patient bed with integrated sensing, which can be useful for patient monitoring. The integrated monitoring bed can automatically monitor patient movement, respiration rate, and/or pulse rate, etc. Certain exemplary embodiments can combine an interferometric integrating fiber optic sensor, matched spatial filtering to potentially optimize signal to noise ratio, a low cost laser pointer, a low cost digital camera, a computer such as a portable laptop PC (or other information device), and/or software, etc. Monitoring patient movement can help determine whether externally induced changes of position might be useful to prevent the occurrence of bedsores.

Certain exemplary embodiments provide a means, integrated into a patient bed, to monitor patient respiration rate, heart rate, and/or amount of movement in a continuous and nonintrusive manner. Certain exemplary embodiments provide a monitoring carpet and/or pad that can be utilized to

monitor the physical activity of elderly patients and/or to alert caregivers when potentially injurious events, such as falls, occur.

Certain exemplary embodiments can facilitate the automation of health care resulting in the potential reduction of certain medical errors. Certain exemplary embodiments can monitor movement of bed-ridden patients thereby limiting the possibility of bedsores developing. Certain exemplary embodiments can monitor movement of an individual on a carpet or pad. If an individual does not move for a predetermined period of time, certain exemplary embodiments permit automated notification of that fact.

A patient's vital signs can be monitored using periodic and/or intrusive monitoring wherein a health care practitioner manually monitors patients vital signs using separate monitoring equipment. With the ever-increasing average age of the population and decreasing number of nursing and other health care support personnel, it can be desirable to automate biomedical measurements thereby freeing up medical staff to concentrate on critical care. Certain automations can be achieved via use of optical fiber sensing technology.

When a pulse of light is transmitted through an optical fiber, the energy can follow a number of paths that cross the fiber's longitudinal axis at different angles. A group of paths that cross the axis at the same angle is known as a mode. The lowest order mode, which is also known as the fundamental mode and the LP_{01} mode, is the mode in which light passes substantially parallel to the fiber axis. In modes other than the fundamental mode, known as high order modes, the light bounces from one side to the other all the way down the fiber. Fibers that have been designed to support only one mode with minimal loss, the fundamental mode, are known as single mode fibers. A multi-mode fiber is a fiber whose design supports multiple modes, and typically supports over 100 modes.

In certain exemplary embodiments, a monochromatic light source, such as a laser diode, can input coherent light into a multi-mode optical fiber segment that is subject to environmental perturbations. The coherent light, as it travels through the core, can assume different modes, including a lowest order mode and at least one higher order mode. The various modes can constructively and destructively interfere to produce a characteristic speckle pattern that can be projected through a spatial filter onto a photo-detector. In its simplest form, the spatial filter can be defined by a light-blocking and/or light-absorbing sheet having one or more apertures, such as circular holes, that pass a subset of the speckle pattern to the photodetector. The signal output of the photodetector can vary in response to the variation in the intensity distribution of that portion of the speckle pattern passed to the photodetector by the spatial filter. The output of the photodetector can be provided to a signal processor with the change in the intensity distribution functionally related to the sensed perturbations.

Certain sensing techniques for detecting changes in inter-mode interference patterns in response to external environmental perturbations are described in Spillman et al., "Statistical Mode Sensor for Fiber Optic Vibration Sensing Applications", *Applied Optics* 28, No. 15, 3166-3176, 1989, which is incorporated herein by reference in its entirety. Such sensing techniques are not believed to have been previously used in an integrated monitoring system for monitoring patients' vital signs.

Certain exemplary embodiments relate to an integrated monitoring bed for monitoring patient vital signs and/or

activity level, and/or to an integrated monitoring carpet/pad for monitoring patient vital signs and/or activity level.

In certain exemplary embodiments, the bed can utilize a sensing technique comprising a multimode fiber optic sensor. Optical energy transmitted through the core of an optical fiber, either a single or multi-mode core, can be affected by physical perturbations of the fiber. The physical perturbation can alter the index of refraction of the core-material and/or the differential indices between the cladding and the core in such a way that the optical energy transmitted through the core can be changed. The physical perturbation can be caused by tension- or compression-induced strain and/or strain induced by bending the fiber about a small radius (i.e., micro-bending) or large radius bending (i.e., macro-bending). Accordingly, an optical fiber can be used as a sensor to measure a physical parameter by correlating changes in the output energy with the environmental perturbations.

The energy output from the sensing fiber can be analyzed, for example, in terms of quantitative changes in intensity, wavelength, and/or polarization states. In a more sophisticated context, the output light can be interferometrically compared against a reference source to provide an interferometer pattern that can be empirically correlated with the fiber-perturbing parameter. In the interferometric context, e.g., a Mach-Zender interferometer, coherent source light can be passed through reference and sensing fibers with the light from the two paths combined to form an interferometric pattern that can be analyzed to provide information that is functionally related to an external perturbation affecting the sensing fiber path.

Certain exemplary embodiments can provide a multi-mode optical fiber sensor and/or method for measuring physical perturbations using interferometric parameter analysis of perturbation-affected light propagated through a multi-mode optical fiber. Certain exemplary embodiments can provide a multi-mode optical fiber sensor and/or method that reduces the optical fiber requirements in an application by providing a multi-function multi-mode optical fiber in which the measurement of physical perturbations using interferometric parameter analysis can be performed in conjunction with other functions, including data transmission, communications, control, and/or telemetry. Certain exemplary embodiments can provide a multi-mode optical fiber sensor and method in which coherent monochromatic radiation from an optical energy source passes through a multi-mode optical fiber that is subjected to an external perturbation. As the light is conducted through the core, the various modes can constructively and destructively interfere with one another with the projected output having a characteristic inter-modal "speckle" pattern. A detector, such as a two-dimensional staring array, can output an electrical signal in response to the intensity distribution of the speckle pattern. As the fiber or a segment thereof is perturbed, the inter-modal interference pattern and/or the intensity distribution can change in a manner functionally related to the perturbation. The corresponding output of the detector can be analyzed by a signal processor to provide a signal output representative of the perturbation.

In certain exemplary embodiments, the output light from the multi-mode optical fiber can be projected onto a multi-pixel CCD array. As the CCD array is scanned, its outputs can be sent to a signal processor that converts the individual pixel output into a corresponding digital value and/or stores the digitized array output as two successive data frames. The absolute value of the change between corresponding pixel

data points in the two data frames can be summed to provide a signal output that is functionally related to the sensed perturbations.

In certain exemplary embodiments, a fiber perturbation region or zone can be defined in which the multi-mode fiber optic sensor is sensitive to perturbation only within the defined region, for example, by providing single mode input and output optical fiber with a intermediate multi-mode optical fiber that is subjected to and senses the perturbations. The light can be output through a spatial filter and/or one or more lenses, such as a $\frac{1}{4}$ pitch gradient index rod lens, to another multi-mode optical fiber segment that can carry the light to the photodetector for processing.

Certain exemplary embodiments can provide a multi-mode optical fiber sensor in which the constructive and destructive interference of coherent light in a multi-mode fiber provides optical information useful in providing a signal that is functionally related to the sensed perturbation. Additionally, the sensing optical fiber can be used to also transmit other data, such as communications, control, telemetry, etc., on wavelength bands outside that used to provide perturbation sensing to provide a multi-function optical fiber.

FIG. 1 is a block diagram of an exemplary embodiment of a multimode fiber optic sensor **1000**. Light from a coherent light source **1100** can be coupled to a multimode optical fiber **1200**. Light exiting fiber **1200** can form a complex speckle pattern due to intermodal interference. If fiber **1200** is perturbed, such as by a perturbation **F**, fiber **1200** can experience mechanical flexing and/or bending, which can cause the distribution of power in the pattern to change but not the total power. In other words, some speckles decrease in power while others increase in power during perturbation, but the total power is unaffected. Light can be output from fiber **1200** and its speckle pattern can be sensed by to a photodetector **1300**, such as a photodetector array, a charge coupled device (CCD), complementary metal oxide semiconductor (CMOS) device, and/or a spatial detector array. Photodetector **1300** can generate a signal **1400**, which can be processed by a signal processor **1500**. The signal processor can sample the whole speckle pattern and/or any portion thereof, and/or can store any portion of the pre-sampled or sampled pattern in a memory device. The pattern can be sampled again and the sum of the absolute values of the intensity changes seen by the pixels of the array can be computed and/or output. The process can then be repeated.

If the integrated perturbation is symbolized as P , and time is symbolized as t , then it has been shown that fiber output is proportional to the absolute value of dP/dt or $\Delta P/\Delta t$, such that for any sensor output at frequency w , the perturbation causing that output would be at $w/2$. Such a fiber is sometimes referred to as a Statistical Mode (STM) sensor.

It has also been shown in Spillman and Huston, "Scaling and Antenna Gain in Integrating Fiber Optic Sensors", Journal of Lightwave Technology 13, No. 7, 1222-1230, (1995), which is incorporated herein by references in its entirety, and in Huston et al., "Monitoring Microfloor Vibrations with Distributed Fiber Optic Sensors", Proc. SPIE 3671, 118-125, 1999, which is incorporated herein by reference in its entirety, that the signal to noise ratio of an integrating sensor can be significantly improved by matching the spatial pattern of the integrating sensor to the parameter field of interest (e.g., via matched filtering and/or preprocessing). It has been discovered that the spatial distribution of the sensor can be matched to the distribution of

displacement produced by, for example, respiration and/or heartbeat, thereby improving the signal to noise ratio of the sensor.

FIG. 2 is a block diagram of an exemplary embodiment of an integrated monitoring device **2000** that can comprise an STM sensor. Light from a coherent optical source **2100**, such as a laser pointer, can be coupled into a multimode optical fiber **2200**, which can be held stationary by a first mechanical fiber/source coupling element **2150**. That portion of fiber **2200** positioned between coupling element **2150** and a target region **2320** of the bed **2300** can be contained within a first mechanical damping element **2220**. The sensing region **2240** of fiber **2200** can be spatially distributed and/or configured in a pattern **2280** chosen to optimize response to respiration, heart rate, and/or movement. For example, for respiration, target region **2320** might be generally defined between an expected position on bed **2300** of the shoulders of a patient and an expected position on bed **2300** of the hips of the patient. Thus, sensing region **2240** and/or pattern **2280** can be generally placed within, on, and/or adjacent, target region **2320**. Pattern **2280** of sensing region **2240** can be serpentine, spiral, irregularly meandering, etc., and can include as many curves and/or turns as needed, and/or can be distributed over as large a percentage of target region **2320** as needed, to optimize response to a targeted vital sign and/or other perturbation. Because the spatial distribution of pattern **2280** and/or sensing region **2240** can be matched to a targeted perturbation, pattern **2280** and/or sensing region **2240** of fiber **2200** can be considered to be a spatial filter.

Fiber **2200** can enter a second mechanical damping element **2260** and can extend to a second mechanical coupling element **2450** that can hold an end of fiber **2200** in the appropriate stationary position to optimally excite a two dimensional photodetector array **2400**, such as a digital camera. Individual pixel intensities then can be transmitted from photodetector **2400** to a computer **2500**, such as a laptop personal computer, for processing as indicated herein.

Fiber **2200**, which can serve as a filter fiber-sensing element, can alternatively be disposed in a carpet or pad (not shown). Pattern **2280** and/or sensing region **2240** of fiber **2200** can be determined by the needs of the application. The upper region (above the legs of a patient) of a monitoring bed can be the only target region **2320** covered by sensing region **2240**, or sensing region **2240** can cover the entire patient resting region of a monitoring bed **2300**. In certain exemplary embodiments, one or more additional integrating fiber optic sensors can be added to the integrated monitoring bed, if desired for additional sensitivity and/or to target other types of perturbations. Alternatively, the entire area of a carpet or pad can correspond to target region **2320** according to the desired application.

A number of experimental runs have been made with test subjects in the four most typical sleep positions, i.e., on back, stomach, and left and right fetal positions. FIG. 3 is a plot **3000** of discrete Fourier transformed data generated by a test subject lying on her stomach in an exemplary embodiment of an integrated monitoring bed depicted in FIG. 2 and utilizing an STM sensor. The frequency axis has been corrected for the fact that the sensor output produces signals at twice the frequency of the perturbation. Although the system was not optimized when the measurements were made as, with respect to FIG. 3, the sampling rate was too high, signals corresponding to both the respiratory rate **3100** and the heart rate **3200** can be seen clearly.

In certain exemplary embodiments, any generic long gauge length sensor, fiber optic or otherwise, can be used as

a perturbation sensor. In terms of fiber optic technology, some of the sensors that can be used can be based on intermodal interference, mode angle shifting, single mode polarimetric shifts, single mode interferometers (Mach-Zehnder, Michaelson), microbending, arrays (serial) of Fabrey-Perot cavities, and/or arrays (serial) of Bragg gratings, etc.

Certain exemplary embodiments can utilize a sensor based on mode angle shifting, or a High Order Mode Excitation (HOME) sensor, which can output a signal that is proportional to a fiber perturbation. FIG. 4 is a side view of an exemplary embodiment of a fiber portion 4000 of such a sensor, which can comprise a multimode optic fiber 4200, into which light 4100 is injected at a non-zero incidence angle β , as measured from the longitudinal axis L of the fiber. That is, rather than being introduced exactly parallel to longitudinal axis L, the light has a radial component as well. This means that the light output 4300 from fiber 4200 will be in the shape of a cone, having a lighted portion 4320 and an unlighted portion 4340. When fiber 4200 is perturbed however, the modes of the light can change, potentially shifting into higher order modes and/or lower order modes. Either type of shift can cause the dimensions and/or shape of lighted portion 4320 and/or unlighted portion 4340 to change. Changes in dimensions and/or shape of lighted portion 4320 and/or unlighted portion 4340 can be detected by a photodetector, such as a pixelated detector (e.g., digital camera, CCD detector, CMOS detector, etc.) and/or a non-pixelated detector (e.g., a large area photodetector). Thus, a photodetector can be positioned, for example, within a circular area normally surrounded and bordered by an annulus created by higher order modes. The photodetector can detect perturbations that result in the excitation of, coupling of, and/or shifting to, lower order modes the light of which is incident within the circular area.

FIG. 5 is a front view of an exemplary projection 5000 on a flat screen 5100 of an output 4300 from the exemplary embodiment of FIG. 4. Projection 5000 can comprise an inner unlighted portion 5200, an outer unlighted portion 5300, and a lighted portion 5400. If the fiber is circular in longitudinal cross-section and flat screen 5100 is oriented perpendicular to the longitudinal axis of the fiber, then unlighted portion 5200 can be circular and/or lighted portion 5400 can be annular.

When the fiber pattern on the monitoring bed is perturbed by motion due to respiration or heartbeat, the inner radius and/or outer radius of the annulus changes, so that if a spatial filter is used that only intercepts a portion of the annular pattern of light and allows it to pass to a detector, an output signal will result containing information about the perturbation. For example, assuming that the outer radius of the annulus increases due to a perturbation, if a spatial filter only passes light that intercepts at least a portion of the area defined only by the increased outer radius, then the fact of the perturbation can be sensed. That is, the spatial filter can pass light that falls within a sector defined between the pre-perturbation outer circumference and the perturbation-caused outer circumference. Likewise if the perturbation decreases a radius, diameter, and/or circumference of the annulus, the spatial filter and/or signal processor can detect the resulting change in the projected light pattern and/or intensity.

FIG. 6 is a block diagram of an exemplary embodiment of a system 6000 that comprises a HOME sensor. In FIG. 6, an optical fiber 6100 can output a light pattern 6200, such as a speckle pattern, which can be projected onto and through a spatial filter 6300 onto a photodetector 6400. The spatial

filter 6300, in a simple physical form, can be fabricated from a opaque sheet having one or more apertures so that a portion of the speckle pattern, indicated generally at 6250, is blocked and a portion or subset 6270 thereof is allowed to pass to the photodetector 6400. Assuming a constant light input to fiber 6100, the intensity of the total circular speckle pattern 6200 remains substantially constant over time, even when fiber 6100 is perturbed, because the average increase in intensity of some of the speckles will be statistically averaged with the average decrease in intensity of other of the speckles. Accordingly, the spatial filter 6300 can function to expose only a portion or subset of the speckle pattern 6200 to the photodetector 6400, so that a change in intensity can be detected. In general, the subset of the speckle pattern 6200 provided by the spatial filter 6300 to the photodetector 6400 can be sufficiently large so that an adequate signal-to-noise ratio is obtained and sufficiently small so that statistical averaging effects do not prevent discrimination of the perturbation effect in the speckle pattern 6200. The shape of the aperture of the spatial filter 6300 is shown in FIG. 6 as an annular opening 6350, although the shape of the aperture or apertures in the spatial filter 6300 may be varied, such as for example, to form a predetermined rectangular matrix of circular holes. The photodetector 6400 can output an electrical signal in response to the intensity of the subset 6270 of speckle pattern 6200 imaged onto the photodetector 6400 through the spatial filter 6300 so that variations in the intensity will provide a corresponding output.

A signal processor 6500 can accept the output of the photodetector 6400 and processes the signal to obtain an information signal functionally related to the perturbation. Since any movement of optical fiber segment 6100 can cause a change in the intensity of the speckle pattern 6200 imaged onto the photodetector 6400, the movement of optical fiber segment 6100 can cause a corresponding change in the signal output of the photodetector 6400. The processing provided by signal processor 6500 can include any of formatting, source encoding, encrypting, channel encoding, multiplexing, modulating, frequency spreading, transmitting, receiving, frequency despread, demodulating, sampling, detecting, demultiplexing, channel decoding, decrypting, source decoding, synchronization, analyzing, comparing, converting, transforming, Fourier transforming, interpreting, monitoring, and/or notifying, etc.

FIG. 7 is a block diagram of an exemplary embodiment of an STM and/or HOME system 7000. As shown, an optical source 7100 can couple coherent radiation into a single-mode optical fiber segment 7200 that is coupled at 7250 to a multi-mode optical fiber 7300 that is subjected to the perturbations F to be sensed, thereby reducing error from undesired vibrations. After the desired perturbation F has been sensed by the multi-mode optical fiber segment 7300, the complex interference pattern is output from the multi-mode optical fiber segment 7300 through a spatial filter 7400. A subset of the complex interference pattern passes through the spatial filter 7400 and is focused through a lens 7500 into a multi-mode optical fiber segment 7600. The complex interference pattern is transmitted along the multi-mode optical fiber segment 7600 to a photodetector 7700, which outputs a signal in response to the intensity of the subset of the complex interference pattern passed by the spatial filter 7400. The signal is output to a signal processor 7800 for analysis in a manner analogous to that described above for the embodiment of FIG. 6.

FIG. 8 is a block diagram of an exemplary embodiment of a system 8000. As shown therein, coherent, monochromatic radiation can be provided to a multi-mode optical fiber

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segment **8100**. The complex interference pattern produced by the optical fiber segment **8100** can be output onto a CCD array **8200** as a characteristic speckle pattern **8300**. The CCD array **8200** can be located a sufficient distance from the output end of the optical fiber segment **8100** so that a pixel on the CCD array **8200** is smaller than an average speckle feature; each pixel thereafter can generate a signal in response to the intensity of radiation incident on that pixel.

A signal processor **8400** can accept the output of the CCD array **8200** and can analyze the information in a frame-by-frame manner with between a first frame and its immediately preceding frame providing information that is functionally related to the perturbation. More specifically, the intensity of the energy sensed by each pixel of the CCD array **8200** can be digitized by a digitizer **8420** and/or stored in a first frame buffer **8430**. This initial frame data can be transferred to a frame delay buffer **8440**, which can hold the frame data for a selected time period, as another data frame is stored in the first data frame buffer **8430**. The initial frame data in the frame delay buffer **8440** then can be transferred to the second data frame buffer **8450**. Accordingly, a preceding $(n-1)^{th}$ data frame can be held in the data frame buffer **8450** and a subsequent n^{th} data frame can be held in the data frame buffer **8430**. Each buffer can take the form of a conventional memory with multi-bit memory locations that correspond to pixels in the CCD array **8200**. A differencing circuit **8460** then can compare the contents of the data frame buffers **8430** and **8450** on a pixel-by-pixel basis and can convert the intensity differences into corresponding absolute values by an absolute value circuit **8470**, which circuit can include memory locations that correspond to pixels of the CCD array **8200**. Lastly, the changes in intensities of the pixels of the CCD array **8200** can be accumulated in a summing circuit **8480** to obtain a final value, which can be output to a memory, a recording device, and/or a display. As successive data frame differences are determined, the final value output will vary as the sensing fiber segment **8100** is perturbed. Thus, the signal processor **8400** can precisely measure the perturbation of the optical fiber segment **8100** by measuring the change in intensity of each individual speckle of the speckle pattern **8300** on the CCD array **8200**.

As in the case of the embodiment of FIG. 8, a subset or portion of the speckle pattern **8300** can be evaluated to provide information functionally related to the perturbation. Although an physical spatial filter can be employed in a manner analogous to that of FIG. 7, the same functional result can be obtained in the embodiment of FIG. 8 via a virtual spatial filter **8410** of signal processor **8400** that disregards or does not pass the output of a selected percentage and/or selected spatial portion of the pixels of the CCD array **8200** so that statistical averaging will not affect the ability to discriminate perturbations in the speckle pattern **8300**.

FIG. 9 is a block diagram of an exemplary embodiment of a wireless optical fiber sensing system **9000**, which can include two portions: a remote portion that can comprise a light source, sensing fiber, CCD camera and wireless transmitter; and a local portion (not shown) composed of wireless receiver and processing laptop.

The remote portion can include a remote wireless module **9100**. External to module **9100**, an power source **9210**, such as an alternating current approximately 110–120 volt power source, can provide electrical power to an alternating current to direct current adapter **9220**, which can plug in to module **9100** to provide direct current to the light source, camera **9400**, and/or wireless transmitter **9500**.

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Within module **9100**, a direct current voltage regulator **9230** can regulate voltage to about 2.5 volts, and provide current to a driver **9240** of an optical source **9310**, such as a laser diode. Light **9320** can be produced and emitted by optical source **9310**. The optical output of optical source **9310** can be coupled to a segment of sensing fiber **9350** via an FC mating sleeve **9330** and a bare fiber adapter **9340**. Similarly, sensing fiber **9350** can be mechanically coupled to module **9100** via bare fiber adapter **9360** and FC mating sleeve **9370**. Light **9380** output by fiber **9350** can be received by a CCD camera **9400**. Sampled frames of the far-field speckles perceived by camera **9400** can be sent to the local portion through a wireless transmitter **9500**.

FIG. 10 is a plot **10000** of power versus frequency data generated by an exemplary embodiment of a HOME optical fiber sensor. The frequency data was obtained via Fourier transform. The plot shows a peak **10100** at about 11 cycles/minute, which corresponds to the respiration rate of the patient.

FIG. 11 is a plot of power versus frequency data generated by an exemplary embodiment of a HOME optical fiber sensor. The frequency data was obtained via Fourier transform. The plot shows a peak **11100** at about 10–15 cycles/minute, which corresponds to the respiration rate of the patient, and a peak at about 55–60 cycles/minute, which corresponds to the heart rate of the patient. FIG. 12 is a plot correlating calculated respiration rate vs. actual respiration rate for data plotted in FIG. 11.

FIG. 13 is a block diagram of an exemplary embodiment of a wireless optic fiber sensing system **13000**. A light source **13100** can couple coherent light to an optical fiber **13200** which is distributed in a predetermined pattern on, above, and/or adjacent a human support structure **13300**, such as a bed, mattress, mattress pad, chair, seat, carpet, carpet pad, and/or floor, etc. In certain exemplary embodiments, the optical fiber can be a 200 micrometer core silica multimode optical fiber arranged in two sinusoidal overlapping patterns arranged orthogonal to each other so that the fiber in each pattern crosses the fiber in the other pattern at an angle of 90 degrees. The light source can be, for example, a DIY laser pointer from Laser Magic Co. of Costa Mesa, Calif., which can provide an output of 5 mW @ 645 nm. Output from optical fiber **13200** can be detected by a photodetector **13400** and an electrical signal generated thereby can be provided to a wireless transmitter **13500**, which can output an electromagnetic signal **13550** from a first zone **13600**, such as a patient's room, to a second zone **13700**, such as a nurse's station. The photodetector and wireless transmitter can be provided as a module, such as for example a GrandTec RFC-3000 wireless CCD module (provided by GrandTec USA of Dallas, Tex.), potentially with an accompanying wireless receiver. The electromagnetic signal **13550**, which can be transmitted at, for example, about 2.4 GHz, can be received by a wireless receiver **13800** and provided, for example via a USB 2.0 interface, to an information device **13900**, which can comprise a signal processor. The receiver, information device, and/or signal processor can potentially handle signals from multiple sensors and/or transmitters. The sampling rate can be, for example, about 30 frames/second. The information device can run a software program designed for processing received signal and/or data encoded therein, calculating appropriate values, such as the Sum of Pixel Differences (SPD) values of adjacent frames, and rendering (i.e., making perceptible) the SPD values in real time possibly in combination with the received frames. The software program can be written in any computer language or tool, such as Visual C++ 6.0 by Microsoft of Redmond,

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Wash. The software program can automatically load a default video source that is coupled to the information device. The software program can save and/or output the SPD values to a predetermined and/or user-specified drive and/or file. The saved file can be in any format, including text, Excel, etc. The software program can provide a graphical user interface.

FIG. 14 is an exemplary user interface 14000 for a wireless optical fiber speckle sensing system. User interface 14000 can include a wide variety of user interface elements, such as an image 14100 of the detected light incident upon the photodetector, the light received by the signal processor, and/or the light processed by the signal processor after filtering and/or preprocessing. Additional user interface elements can include a video source feature and/or parameter button 14200, a frame indicator and/or control 14300, a Sum of Pixel Difference (SPD) indicator and/or control 14400, a maximum SPD indicator and/or control 14500, an autoscale control 14600, an SPD scale indicator and/or control 14700, and/or a plot 14800 of SPD intensity versus time and/or location, etc.

FIG. 15 is an exemplary user interface 15000 for advanced video source features and/or parameters. User interface 15000 can include a wide variety of user interface elements, such as tabs 15100, 15200, 15300, 15400 for switching between various groups of video source features and/or parameters. User interface 15000 also can include a video standard indicator and/or control 15500, a maximum bandwidth indicator and/or control 15600, a consumed bandwidth indicator 15700, a horizontal offset indicator and/or control 15800, and/or a vertical offset indicator and/or control 15900, etc.

FIG. 16 is an exemplary user interface 16000 for capture source features and/or parameters. User interface 16000 can include a wide variety of user interface elements, such as video device selector 16100 and/or video source indicator and/or control 16200.

FIG. 17 is an exemplary user interface 17000 for video device settings. User interface 17000 can include a wide variety of user interface elements, such as indicators, selectors, and/or controls for brightness 17100, contrast 17200, hue 17300, saturation 17400, sharpness 17500, white balance 17600, gamma 17700, and/or backlighting 17800, etc.

FIG. 18 is an exemplary user interface 18000 for camera controls. User interface 18000 can include a wide variety of user interface elements, such as indicators, selectors, and/or controls for zoom 18100, focus 18200, exposure 18300, iris 18400, tilt 18500, pan 18600, and/or roll 18700, etc.

FIG. 19 is an exemplary user interface 19000 for stream settings. User interface 19000 can include a wide variety of user interface elements, such as indicators, selectors, and/or controls for resolution 19100, pixel depth and/or compression 19200, and/or size 19300, etc. FIG. 20 is an exemplary output data list 20000, which can display a plurality of SPD values 20100. FIG. 21 is structural diagram of an exemplary software program 21000.

FIG. 22 is a flowchart of an exemplary embodiment of a method 22000. At activity 22100, an optical fiber is spatially distributed in a predetermined pattern for facilitating sensing of a predetermined type of perturbation. For example, a fiber can be distributed on a bed in a pattern that is known to facilitate sensing of a person leaving or entering the bed, a position of the person on the bed, whether the person has rolled lately, a heartbeat of the person, and/or a respiration rate of the person, etc. A fiber can be distributed in a pattern that is known to facilitate sensing of a target, such as a person, animal, and/or vehicle, etc., entering an area and/or

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leaving the area. A fiber can be distributed in a pattern that is known to facilitate sensing of whether a perturbation is caused by a person, an animal, or an object, etc., potentially by virtue of a weight, weight distribution, and/or frequency of impact, etc. The presence of the fiber can be hidden and/or non-intrusive. The fiber can be rugged and/or impervious to liquid contact.

At activity 22200, output of the fiber can be spatially filtered. Such filtering can occur optically and/or digitally. At activity 22300, output of the fiber, such as optical signals, can be detected. At activity 23400, the detected fiber output can be transmitted, such as via an electromagnetic signal, such as a wireless signal. Prior to transmission, the detected output can be formatted, source encoded, encrypted, channel encoded, multiplexed, modulated, and/or frequency spread, etc. At activity 23500, the transmitted signal can be received. The receiver can receive signals from multiple transmitters. At activities 23600 and 23700, the received signal can be processed, which can include frequency despread, demodulating, sampling, holding, digitizing, detecting, demultiplexing, channel decoding, decrypting, source decoding, synchronization, spatial filtering, comparing, summing, calculating, interpreting, and/or analyzing the signal and/or variables encoded therein. For example, the received signal can be processed to determine intensity, power, voltage, current, phase, and/or frequency values, and/or changes therein. Via time division, frequency division, code division, phase division, and/or other division techniques for multiple access and/or multiplexing, multiple signals can be received by a single receiver and/or processed by a single signal processor. Because a least certain such values of the signal can vary with time, particularly due to perturbations of the sensing fiber, at activity 22800, the signal, variable values, and/or received data can be continuously and monitored for statistically significant deviations from predetermined values and/or limits. At activity 22900, a notification can be provided if a deviation is detected. The notification can be provided by any technique and can be in any form. For example, a warning notification can be provided to a nurse if a patient has been immobile for too long and needs to be turned to prevent the formation of bed sores. As another example, a warning can be provided if motion is detected when, where, and/or to an extent not expected, such as for example, if the force, impact, and/or acceleration, etc., of a fallen patient, an intruder, an overweight truck approaching a bridge, seismic movement, and/or vibration, etc., is detected. Any or all detected, processed, monitored, and/or notification data can be logged. Thus, if a notification is provided to a nurse to turn a patient, the system can also log that the turn occurred, thereby providing a validation record of the movement to limit and/or avoid potential liability.

FIG. 23 is a block diagram of an exemplary embodiment of an information device 23000, which can represent any of information device described herein, such as information device 13900 of FIG. 13. Information device 23000 includes any of numerous well-known components, such as for example, one or more network interfaces 23100, one or more processors 23200, one or more memories 23300 containing instructions 23400, and/or one or more input/output (I/O) devices 23500, etc. Via one or more I/O devices 23500, a user interface 23600 can be provided.

As used herein, the term "information device" means any device capable of processing information, such as any general purpose and/or special purpose computer, such as a personal computer, workstation, server, minicomputer, mainframe, supercomputer, computer terminal, laptop,

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wearable computer, and/or Personal Digital Assistant (PDA), mobile terminal, Bluetooth device, communicator, “smart” phone (such as a Handspring Treo-like device), messaging service (e.g., Blackberry) receiver, pager, facsimile, cellular telephone, a traditional telephone, telephonic device, a programmed microprocessor or microcontroller and/or peripheral integrated circuit elements, an ASIC or other integrated circuit, a hardware electronic logic circuit such as a discrete element circuit, and/or a programmable logic device such as a PLD, PLA, FPGA, or PAL, or the like, etc. In general any device on which resides a finite state machine capable of implementing at least a portion of a method, structure, and/or graphical user interface described herein may be used as an information device. An information device can include well-known components such as one or more network interfaces, one or more processors, one or more memories containing instructions, and/or one or more input/output (I/O) devices, one or more user interfaces, etc.

As used herein, the term “network interface” means any device, system, or subsystem capable of coupling an information device to a network. For example, a network interface can be a telephone, cellular phone, cellular modem, telephone data modem, fax modem, wireless transceiver, ethernet card, cable modem, digital subscriber line interface, bridge, hub, router, or other similar device.

As used herein, the term “processor” means a device for processing machine-readable instruction. A processor can be a central processing unit, a local processor, a remote processor, parallel processors, and/or distributed processors, etc. The processor can be a general-purpose microprocessor, such the Pentium III series of microprocessors manufactured by the Intel Corporation of Santa Clara, Calif. In another embodiment, the processor can be an Application Specific Integrated Circuit (ASIC) or a Field Programmable Gate Array (FPGA) that has been designed to implement in its hardware and/or firmware at least a part of an embodiment disclosed herein.

As used herein, a “memory device” means any hardware element capable of data storage, such as for example, a non-volatile memory, volatile memory, Random Access Memory, RAM, Read Only Memory, ROM, flash memory, magnetic media, a hard disk, a floppy disk, a magnetic tape, an optical media, an optical disk, a compact disk, a CD, a digital versatile disk, a DVD, and/or a raid array, etc.

As used herein, the term “firmware” means machine-readable instructions that are stored in a read-only memory (ROM). ROM’s can comprise PROMs and EPROMs.

As used herein, the term “I/O device” means any sensory-oriented input and/or output device, such as an audio, visual, haptic, olfactory, and/or taste-oriented device, including, for example, a monitor, display, projector, overhead display, keyboard, keypad, mouse, trackball, joystick, gamepad, wheel, touchpad, touch panel, pointing device, microphone, speaker, video camera, camera, scanner, printer, haptic device, vibrator, tactile simulator, and/or tactile pad, potentially including a port to which an I/O device can be attached or connected.

As used herein, the term “haptic” means both the human sense of kinesthetic movement and the human sense of touch. Among the many potential haptic experiences are numerous sensations, body-positional differences in sensations, and time-based changes in sensations that are perceived at least partially in non-visual, non-audible, and non-olfactory manners, including the experiences of tactile touch (being touched), active touch, grasping, pressure, friction, traction, slip, stretch, force, torque, impact, punc-

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ture, vibration, motion, acceleration, jerk, pulse, orientation, limb position, gravity, texture, gap, recess, viscosity, pain, itch, moisture, temperature, thermal conductivity, and thermal capacity.

As used herein, the term “user interface” means any device for rendering information to a user and/or requesting information from the user. A user interface includes at least one of textual, graphical, audio, video, animation, and/or haptic elements. A textual element can be provided, for example, by a printer, monitor, display, projector, etc. A graphical element can be provided, for example, via a monitor, display, projector, and/or visual indication device, such as a light, flag, beacon, etc. An audio element can be provided, for example, via a speaker, microphone, and/or other sound generating and/or receiving device. A video element or animation element can be provided, for example, via a monitor, display, projector, and/or other visual device. A haptic element can be provided, for example, via a very low frequency speaker, vibrator, tactile stimulator, tactile pad, simulator, keyboard, keypad, mouse, trackball, joystick, gamepad, wheel, touchpad, touch panel, pointing device, and/or other haptic device, etc.

A user interface can include one or more textual elements such as, for example, one or more letters, number, symbols, etc. A user interface can include one or more graphical elements such as, for example, an image, photograph, drawing, icon, window, title bar, panel, sheet, tab, drawer, matrix, table, form, calendar, outline view, frame, dialog box, static text, text box, list, pick list, pop-up list, pull-down list, menu, tool bar, dock, check box, radio button, hyperlink, browser, button, control, palette, preview panel, color wheel, dial, slider, scroll bar, cursor, status bar, stepper, and/or progress indicator, etc. A textual and/or graphical element can be used for selecting, programming, adjusting, changing, specifying, etc. an appearance, background color, background style, border style, border thickness, foreground color, font, font style, font size, alignment, line spacing, indent, maximum data length, validation, query, cursor type, pointer type, autosizing, position, and/or dimension, etc. A user interface can include one or more audio elements such as, for example, a volume control, pitch control, speed control, voice selector, and/or one or more elements for controlling audio play, speed, pause, fast forward, reverse, etc. A user interface can include one or more video elements such as, for example, elements controlling video play, speed, pause, fast forward, reverse, zoom-in, zoom-out, rotate, and/or tilt, etc. A user interface can include one or more animation elements such as, for example, elements controlling animation play, pause, fast forward, reverse, zoom-in, zoom-out, rotate, tilt, color, intensity, speed, frequency, appearance, etc. A user interface can include one or more haptic elements such as, for example, elements utilizing tactile stimulus, force, pressure, vibration, motion, displacement, temperature, etc.

In certain exemplary embodiments, via one or more user interfaces **23600**, a user can specify, input, view, locate, store, output, manipulate, and/or control, data, variables, parameters, and/or commands related to an operation of an optical sensing system, such as described herein.

We analyzed the applicability of these two techniques for simultaneously detecting patient movement, respiration and heart rate. The perturbation due to respiration and heart rate was modeled as the sum of two cosine functions with the second cosine having an amplitude of 0.1 of the amplitude of the first. The discrete Fourier transform of this modeled signal and the transform of the absolute value of the first derivative of the signal is shown in FIG. **24**. As can be seen,

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the modeled SMS power spectra (fine line) clearly shows the first perturbation (at twice its frequency due to the taking of absolute value) but does not show the second perturbation due to complications from this type of processing. The HOME signal, on the other hand, clearly shows the peaks due to both perturbations at their correct frequencies. The SMS approach allows detection of respiration and heart rate and is more sensitive than the HOME approach, but the HOME approach introduces less distortion due to processing and should allow better signal discrimination.

A number of experimental runs were conducted using both the SMS and HOME sensors. A typical time trace from the SMS sensor is shown in FIG. 25 while its Fourier transform is shown in FIG. 26. FIG. 27 shows how the results vary for patients in different typical sleep positions: on back, on stomach, left fetal and right fetal. The signal peaks are at twice the respiration rate as expected.

A typical time trace using the HOME sensor is shown in FIG. 28, and its power spectrum is shown in FIG. 29. FIG. 11 shows the power spectrum from the HOME sensor when the test subject held his breath for 0.5 of the measurement period. This allowed the heart rate signal to be clearly discerned. Finally, FIG. 12 displays the measured (via the peak in the power spectrum) vs the actual (as determined by patient counting) respiration rates using the HOME sensor.

As can be seen from these results, both the SMS and HOME sensors can be used to detect patient movement and respiration. Only the HOME sensor, however, demonstrated the ability to detect heart rate in this experiment. The SMS sensor, by the nature of its transduction process, will not become saturated, i.e. because it takes the derivative of a signal. The size of the DC component does not affect the sensitivity of this signal processing method. It can therefore detect patient movement and give repeatable results somewhat independently of patient weight. The HOME sensor, on the other hand, could be saturated by perturbations large enough to cause the available propagating mode volume to become completely filled. Both sensors can be low cost, PC compatible, and can be integrated into larger wireless systems.

Still other embodiments will become readily apparent to those skilled in this art from reading the above-recited detailed description and drawings of certain exemplary embodiments. It should be understood that numerous variations, modifications, and additional embodiments are possible, and accordingly, all such variations, modifications, and embodiments are to be regarded as being within the spirit and scope of the appended claims. For example, regardless of the content of any portion (e.g., title, field, background, summary, abstract, drawing figure, etc.) of this application, unless clearly specified to the contrary, there is no requirement for the inclusion in any claim of the application of any particular described or illustrated activity or element, any particular sequence of such activities, or any particular interrelationship of such elements. Moreover, any activity can be repeated, any activity can be performed by multiple entities, and/or any element can be duplicated. Further, any activity or element can be excluded, the sequence of activities can vary, and/or the interrelationship of elements can vary. Accordingly, the descriptions and drawings are to be regarded as illustrative in nature, and not as restrictive. Moreover, when any number or range is described herein, unless clearly stated otherwise, that number or range is approximate. When any range is described herein, unless clearly stated otherwise, that range includes all values therein and all subranges therein. Any information in any material (e.g., a United States patent, United States

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patent application, book, article, etc.) that has been incorporated by reference herein, is only incorporated by reference to the extent that no conflict exists between such information and the other statements and drawings set forth herein. In the event of such conflict, including a conflict that would render a claim invalid, then any such conflicting information in such incorporated by reference material is specifically not incorporated by reference herein.

What is claimed is:

1. A system, comprising:
 - a spatially distributed multimode optical fiber;
 - a photodetector configured to detect optical signals provided from said fiber;
 - a wireless digital module coupled to said photodetector and adapted to wirelessly transmit a wireless signal encoding a plurality of detected variables of the optical signals;
 - a wireless receiver adapted to receive the wireless signal; and
 - a signal processing module coupled to said wireless receiver and adapted to decode and interpret the plurality of detected variables of the optical signals.
2. The system of claim 1, further comprising a coherent optical source optically couplable to said optical fiber.
3. The system of claim 1, further comprising a laser diode optically couplable to said optical fiber.
4. The system of claim 1, further comprising a laser light pointer optically couplable to said fiber.
5. The system of claim 1, further comprising an electronic driver adapted to control light provided to said fiber.
6. The system of claim 1, wherein said fiber is integrating.
7. The system of claim 1, wherein said fiber is spatially distributed with respect to a patient bed for optimized detection of patient movement.
8. The system of claim 1, wherein said fiber is spatially distributed with respect to a patient bed for optimized detection of patient respiration.
9. The system of claim 1, wherein said fiber is spatially distributed with respect to a patient bed for optimized detection of patient heart rate.
10. The system of claim 1, wherein said fiber is spatially distributed with respect to a patient bed for optimized detection of any combination of patient movement, respiration rate, and heart rate.
11. The system of claim 1, wherein said fiber converts higher order modes to lower order modes.
12. The system of claim 1, wherein said fiber converts lower order modes to higher order modes.
13. The system of claim 1, wherein the optical signals comprise a speckle pattern.
14. The system of claim 1, wherein the optical signals comprise a plurality of high order excitation modes.
15. The system of claim 1, wherein the optical signals comprise a plurality of high order excitation modes that are proportional to a perturbation along said fiber.
16. The system of claim 1, wherein said photodetector is optically couplable to said optical fiber.
17. The system of claim 1, wherein said photodetector provides an output proportional an integrated perturbation along said fiber.
18. The system of claim 1, wherein said photodetector comprises a photodetector array.
19. The system of claim 1, wherein said photodetector comprises a digital photodetector.
20. The system of claim 1, wherein said photodetector comprises a digital photodetector array.

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21. The system of claim 1, wherein said photodetector comprises a CCD camera.

22. The system of claim 1, wherein said photodetector comprises a CMOS camera.

23. The system of claim 1, wherein the wireless signal encodes a plurality of digitized images of the optical signals.

24. The system of claim 1, further comprising a high order mode transmission element optically couplable to said optical fiber.

25. The system of claim 1, further comprising a filter configured to pass only lower order modes converted from higher order modes.

26. The system of claim 1, further comprising a filter configured to pass only higher order modes converted from lower order modes.

27. The system of claim 1, further comprising a matched spatial filter.

28. The system of claim 1, further comprising a matched spatial filter adapted to spatially filter light provided to said fiber.

29. The system of claim 1, further comprising a matched spatial filter adapted to filter the optical signals.

30. The system of claim 1, further comprising a matched spatial filter adapted to spatially filter the plurality of detected variables of the optical signals.

31. The system of claim 1, further comprising a matched spatial filter adapted to filter a plurality of digitized images provided by said photodetector.

32. The system of claim 1, wherein said signal processing module is adapted to decode a plurality of digitized images and to interpret one or more variables of the plurality of digitized images.

33. The system of claim 1, wherein said signal processing module provides an output proportional to an absolute value of $\Delta P/\Delta t$, where P is an integrated perturbation along said fiber and t is time.

34. The system of claim 1, wherein said signal processing module is adapted to provide matched spatial filtering of a plurality of digitized images to optimize a signal-to-noise ratio.

35. The system of claim 1, wherein said signal processing module is adapted to process a predetermined portion of the optical signals.

36. The system of claim 1, wherein said signal processing module is adapted to process a portion of the optical signals, the portion associated with a human vital sign.

37. The system of claim 1, wherein said signal processing module is adapted to interpret a frequency of a perturbation of the fiber.

38. The system of claim 1, wherein said signal processing module is adapted to interpret a frequency of a perturbation of the plurality of detected variables.

39. The system of claim 1, wherein said signal processing module is adapted to interpret fluctuations in a speckle pattern of the optical signals.

40. The system of claim 1, wherein said signal processing module is adapted to interpret a conversion of excitation modes of the optical signals in a spatially filtered region.

41. The system of claim 1, wherein said signal processing module is adapted to interpret an incidence of lower order excitation modes of the optical signals in a predetermined spatial region.

42. The system of claim 1, wherein said signal processing module is adapted to interpret an incidence of high order excitation modes of the optical signals in a predetermined spatial region.

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43. The system of claim 1, wherein said signal processing module is adapted to interpret a frequency of a perturbation of the plurality of detected variables, the frequency corresponding to a patient vital sign.

44. The system of claim 1, wherein said signal processing module is adapted to interpret a frequency of a perturbation of the plurality of detected variables, the frequency corresponding to a patient movement.

45. The system of claim 1, wherein said signal processing module is adapted to interpret a change in an optical power of the plurality of detected variables.

46. The system of claim 1, wherein said signal processing module is adapted to interpret a change in angle of an excitation mode of the optical signals.

47. The system of claim 1, wherein said signal processing module is adapted to interpret a change in excitation modes of the optical signals.

48. The system of claim 1, wherein said signal processing module is adapted to monitor the plurality of detected variables of the for a change in a patient's vital sign.

49. The system of claim 1, wherein said signal processing module is adapted to monitor the plurality of detected variables for a change in a patient's movement.

50. The system of claim 1, wherein said signal processing module is adapted to automatically monitor the plurality of detected variables for a change in patient movement, respiration rate, or pulse rate.

51. The system of claim 1, further comprising: a human support structure supporting said fiber.

52. The system of claim 1, further comprising: a human support structure adjacent said fiber.

53. The system of claim 1, further comprising: a mattress adjacent said fiber.

54. The system of claim 1, further comprising: a pad adjacent said fiber.

55. The system of claim 1, further comprising: a carpet adjacent said fiber.

56. The system of claim 1, wherein said system comprises an STM sensor.

57. The system of claim 1, wherein said system comprises a HOME sensor.

58. A method, comprising:

transmitting from a wireless digital photodetector coupled to an fiber optic sensor a signal encoding a plurality of detected variables of optical signals emerging from the fiber optic sensor;

receiving the signal at a wireless receiver;

decoding the signal at a signal processing module coupled to a wireless receiver; and

interpreting the plurality of detected variables of the decoded signal.

59. A method, comprising:

spatially distributing a multimode optical fiber in a predetermined pattern for facilitating sensing of a predetermined type of perturbation;

transmitting optical signals from the spatially distributed integrating multimode optical fiber;

detecting the optical signals at a photodetector; and

wirelessly transmitting a wireless signal encoding a plurality of detected variables of the optical signals.

60. The method of claim 59, further comprising:

receiving the wireless signal at a wireless receiver.

61. The method of claim 59, further comprising: decoding the wireless signal.

62. The method of claim 59, further comprising: decoding the wireless signal at a signal processing module coupled to a wireless receiver.

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63. The method of claim 59, further comprising: decrypting the wireless signal.
 64. The method of claim 59, further comprising: frequency despread the wireless signal.
 65. The method of claim 59, further comprising: demodulating the wireless signal.
 66. The method of claim 59, further comprising: sampling the wireless signal.
 67. The method of claim 59, further comprising: digitizing the wireless signal.
 68. The method of claim 59, further comprising: detecting the wireless signal.
 69. The method of claim 59, further comprising: demultiplexing the wireless signal.
 70. The method of claim 59, further comprising: spatially filtering the optical signals.
 71. The method of claim 59, further comprising: spatially filtering the wireless signal.
 72. The method of claim 59, further comprising: spatially filtering the detected variables.
 73. The method of claim 59, further comprising: Fourier transforming the wireless signal.
 74. The method of claim 59, further comprising: interpreting the wireless signal.

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75. The method of claim 59, further comprising: interpreting the plurality of detected variables.
 76. The method of claim 59, further comprising: monitoring the wireless signal.
 5 77. The method of claim 59, further comprising: monitoring the plurality of detected variables.
 78. The method of claim 59, further comprising: providing notification of a predetermined change in the wireless signal.
 10 79. The method of claim 59, further comprising: providing notification of a predetermined change in the plurality of detected variables.
 80. A machine-readable medium comprising instructions for activities comprising:
 15 decoding a wireless signal obtained from a wireless digital photodetector coupled to an optical fiber spatially distributed in a predetermined pattern for facilitating sensing of a predetermined type of perturbation, the wireless signal encoding a plurality of detected variables of optical signals emerging from the spatially distributed fiber optic sensor; and
 20 interpreting the plurality of detected variables of the decoded signal.

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